



# IMAGE GUIDANCE AND REGISTRATION – PARTICULAR CHALLENGES IN CASE OF RE- IRRADIATION

MARTIN F. FAST

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## ACKNOWLEDGEMENTS / SLIDE CREDITS

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# CONFLICTS OF INTEREST

- Financial and technical support from Elekta AB under research agreements
- NKI-AvL is part of the Elekta Atlantic MR-linac Research Consortium



<https://mrrt.elekta.com/>

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# OUTLINE

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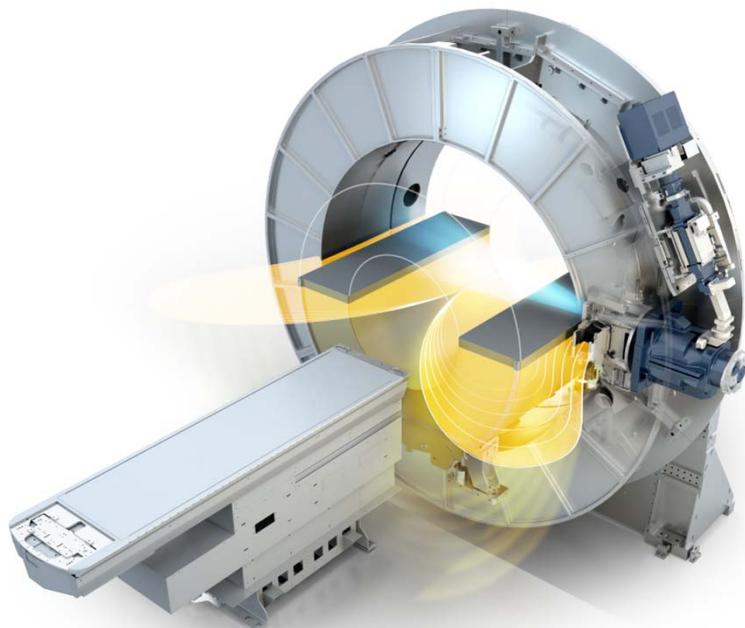
**THE FUTURE IS NOW – MRI-GUIDED RADIOTHERAPY**

**THE WORKING HORSE – CBCT-GUIDED RADIOTHERAPY**

**DOSE ACCUMULATION – READY FOR CLINICAL USE?**

**IMAGE REGISTRATION – CHALLENGES AND OPPORTUNITIES**

# ELEKTA UNITY MR-LINAC



- 1.5 T Philips magnet
- 7 MV linac
- 22x56 cm<sup>2</sup> treatment field
- Real-time cine-MR imaging
- MLC based on Agility design

Photo courtesy: Elekta AB

# ELEKTA UNITY MR-LINAC AT NKI-AVL

## INSTALLATION

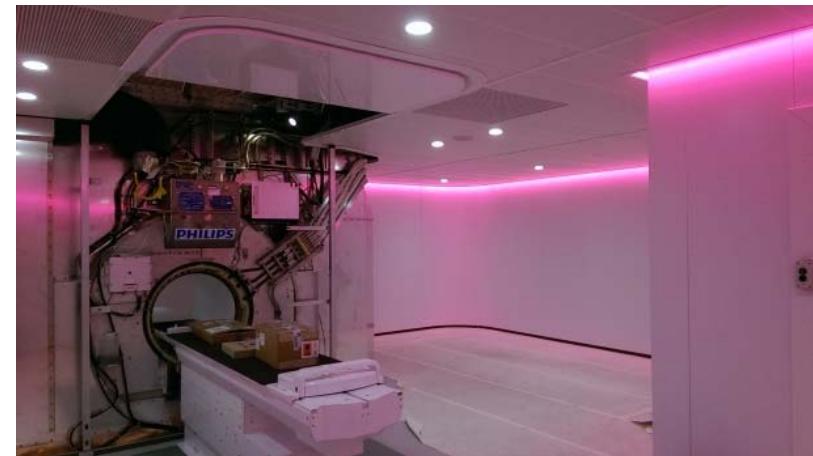
- May 2016

## INITIAL RESEARCH PHASE

- Phantom measurements
- Volunteer imaging
- Patient volunteer imaging

## FINAL UPGRADE

- June-August 2018



# ELEKTA UNITY MR-LINAC AT NKI-AVL

First patient treated TODAY  
(September 6th, 2018)



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# MR-LINAC AT NKI

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## Clinical focus

- Prostate cancer
- Rectal cancer
- *Oligometastases (especially liver)*

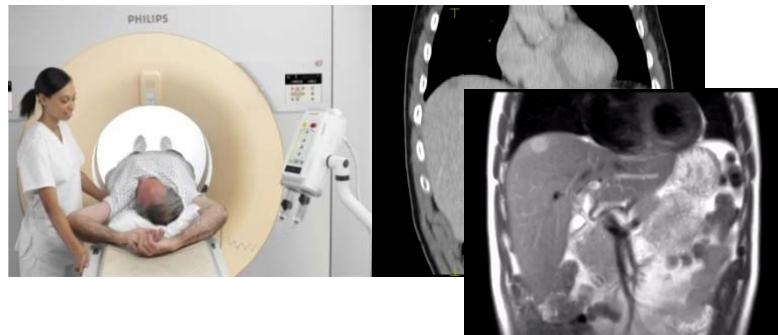
## Technical focus

- EPID dosimetry
- *Practical 4D solutions*
- Quantitative imaging

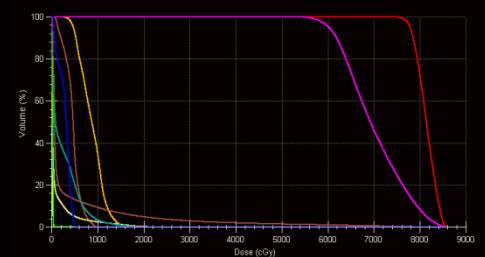
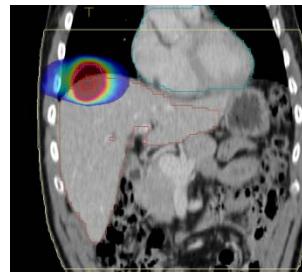
# NKI'S LIVER RT WORKFLOW FOR THE MR-LINAC

## PRE-TREATMENT IMAGING

4D-CT + 4D-MRI



## TREATMENT PLANNING

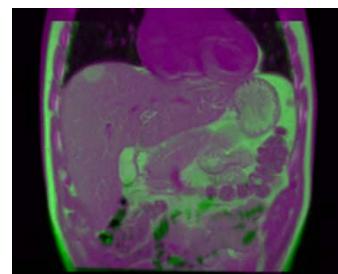


## DAILY IMAGING

4D-MRI



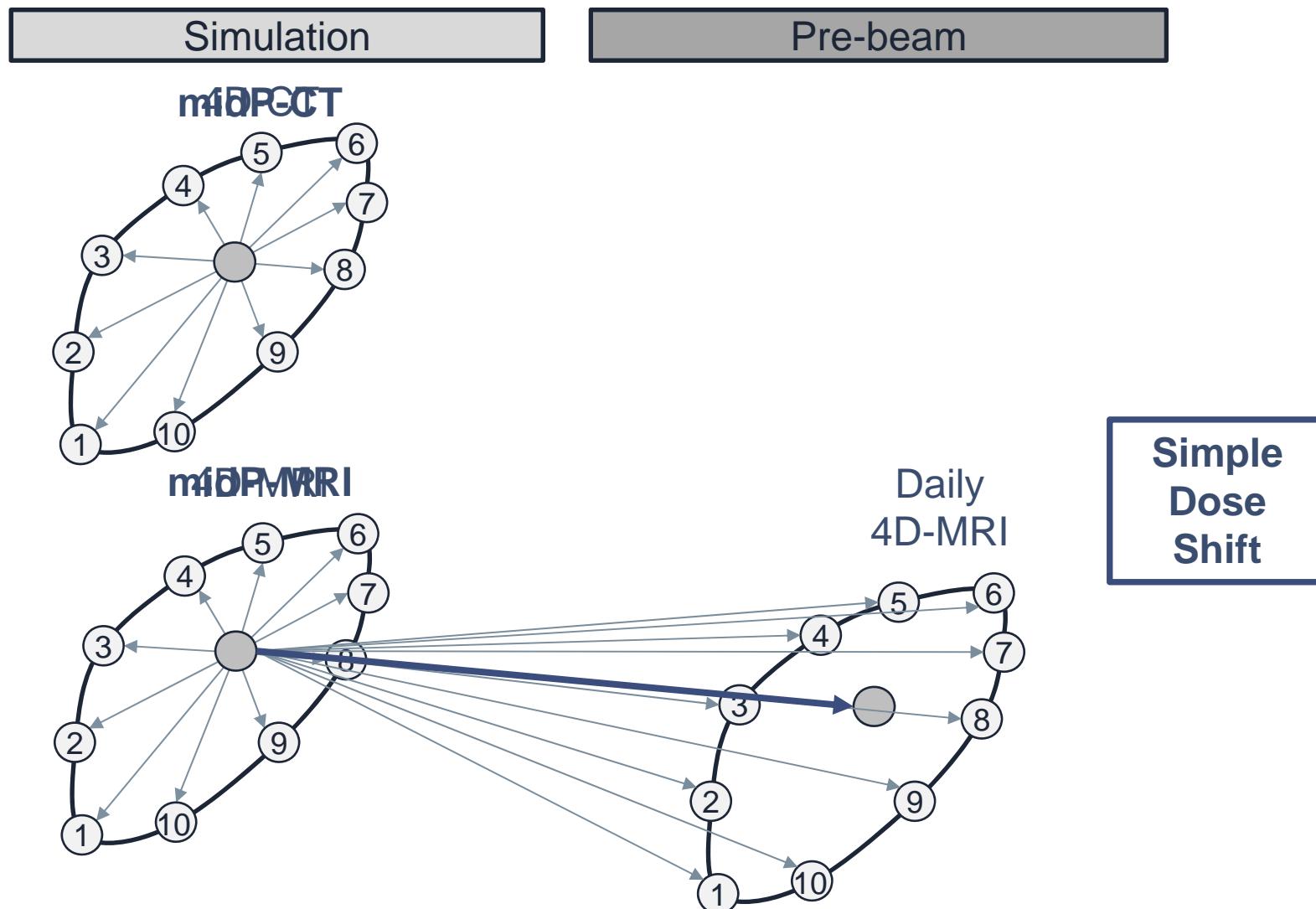
## IMAGE REGISTRATION & PLAN ADAPTATION



## TREATMENT DELIVERY

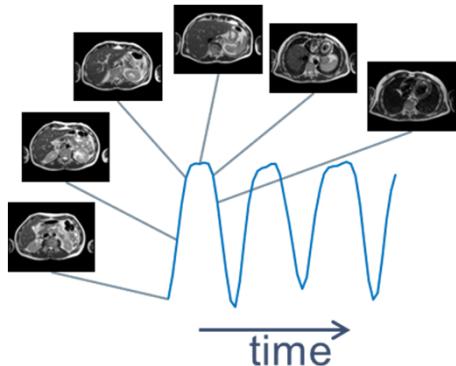


# MID-POSITION STRATEGY ON THE MR-LINAC



# SELF-GATED 4D-MRI

## 2D SEQUENCE



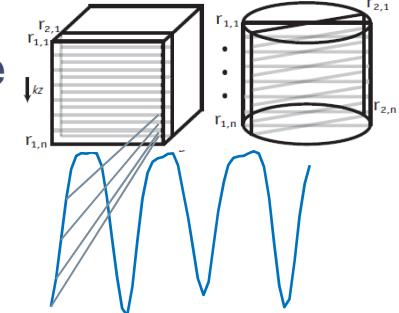
## DATA ACQUISITION

Data from arbitrary respiratory phases



## 3D SEQUENCE

Cartesian Radial



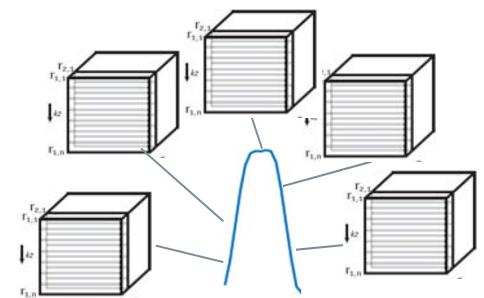
K-space

## RESPIRATORY SIGNAL



## DATA SORTING

To amplitude or phase



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## 4D-MRI ACQUISITION: 2D VS 3D

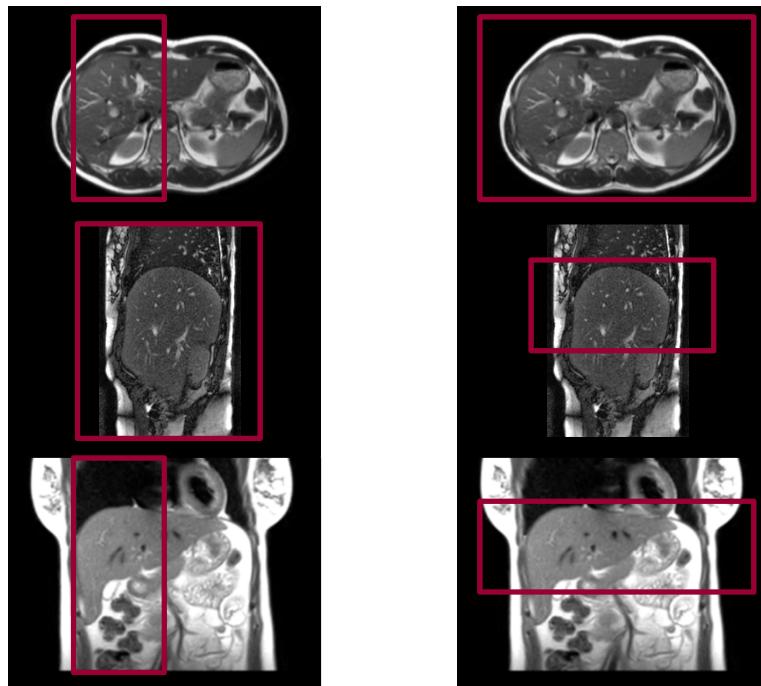
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Acquisition	2D	3D
SNR (spatial resolution)	-	+
Acquisition / reconstruction time	~minutes (3-15min)	<minute ~hours / dedicated reconstruction server
Pulse sequences	Standard	Tailored
Contrasts	T1 or T2 - weighted	T1-weighted

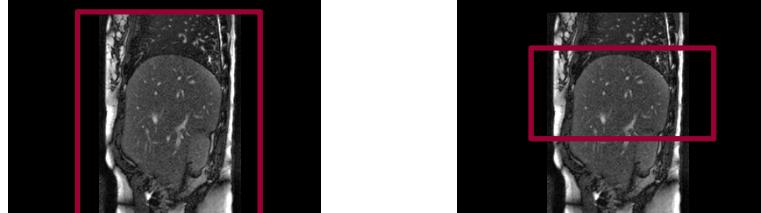
## 2D-BASED 4D-MRI

2D Orientation	Sagittal	Axial	Coronal
CC-motion	In-plane	Out-of-plane	In-plane
FOV coverage / acquisition time	-	+	+

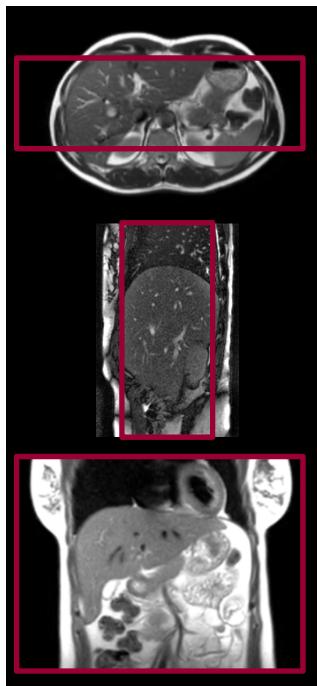
Axial



Sagittal



Coronal



FOV: 25 slices of 5mm, Acq time: ~4min

# AXIAL/CORONAL 4D-MRI



4D-MRI

## Retrospective self-sorted 4D-MRI for the liver

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MR-Linac  
Self-gating

### ABSTRACT

**Purpose:** Daily MRI-guidance is a promising technique for liver cancer treatment. However, the reconstruction time is currently >5 min. **Materials and Methods:** Imaging was performed with a 4D-MRI sequence, repeated a variable number of times. The data were processed by computing corresponding phases and missing data were estimated. The SSIM image quality was assessed as a function of the number of phases. **Results:** SSIM was in good agreement with the ground truth (0.4 ± 0.6% to 37.1 ± 6.6% for 30–100 phases). The RMSD of quantified motion was <10 mm for >10 dynamics. **Conclusion:** For 30 dynamics, the reconstruction time was reduced to 1 min. © 2018 Elsevier

### Clinical Investigation

## A Self-Sorting Coronal 4D-MRI Method for Daily Image Guidance of Liver Lesions on an MR-LINAC

Tessa van de Lindt, MSc, Jan-Jakob Sonke, PhD,  
Marlies Nowee, MD, PhD, Edwin Jansen, MD, PhD, Vivian van Pelt,  
Ulke van der Heide, PhD, and Martin Fast, PhD

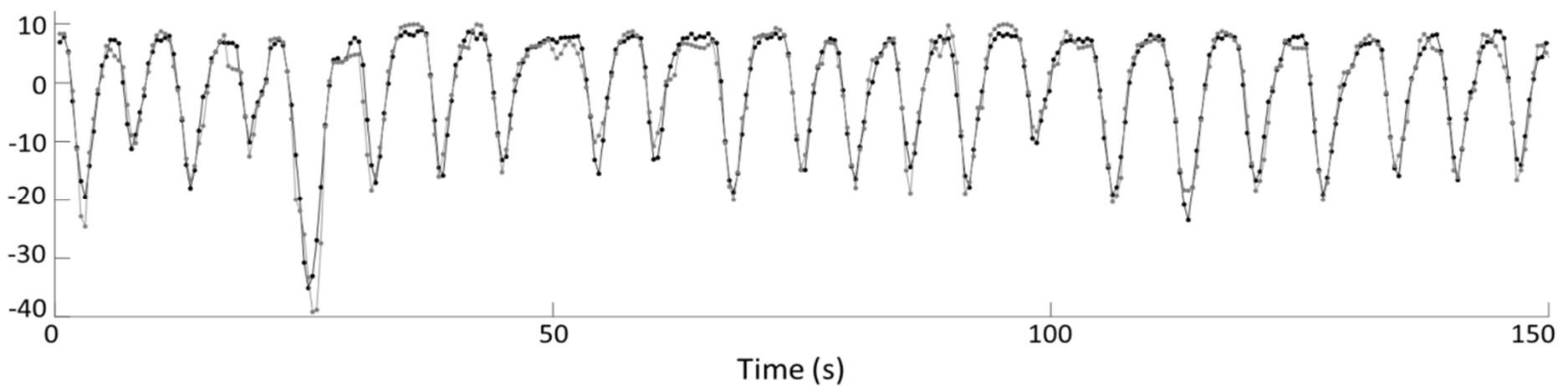
Department of Radiation Oncology, The Netherlands Cancer Institute, Amsterdam, The Netherlands

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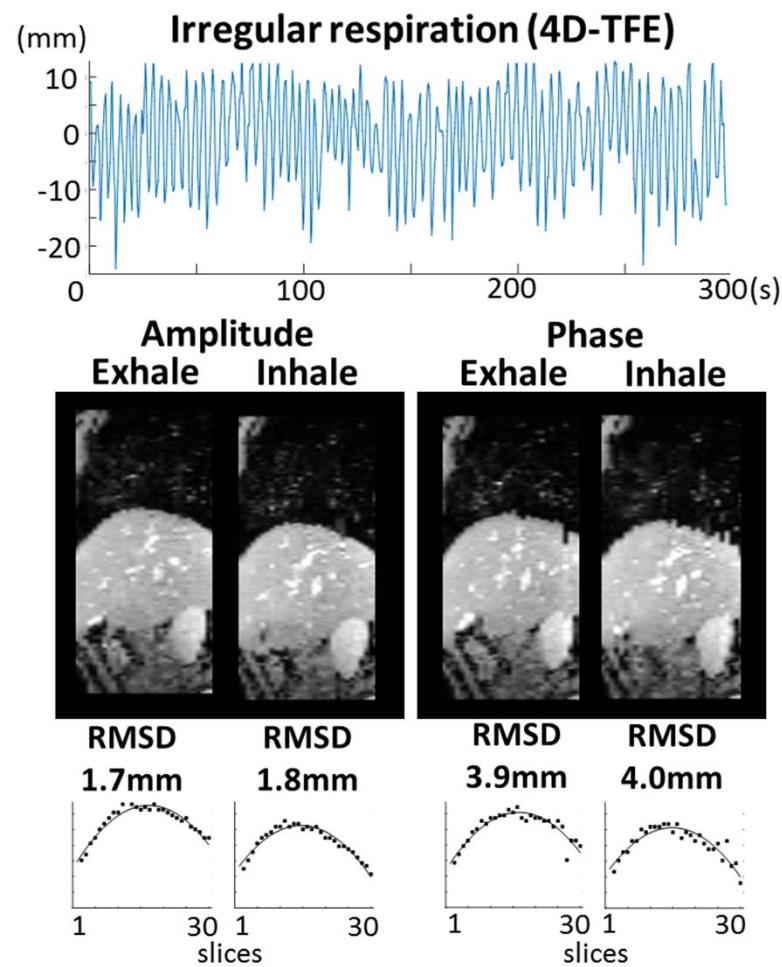
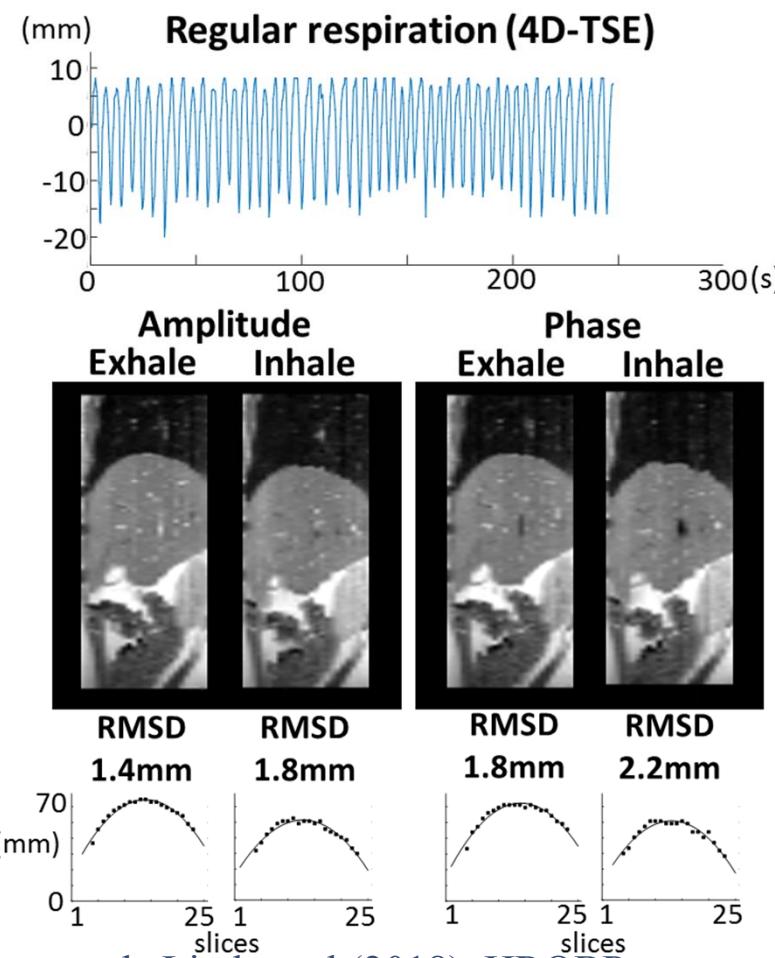
## RESULTS: SELF-SORTING SIGNAL ANALYSIS



**Table 1: Image-based self-sorting signal vs navigator signal results**

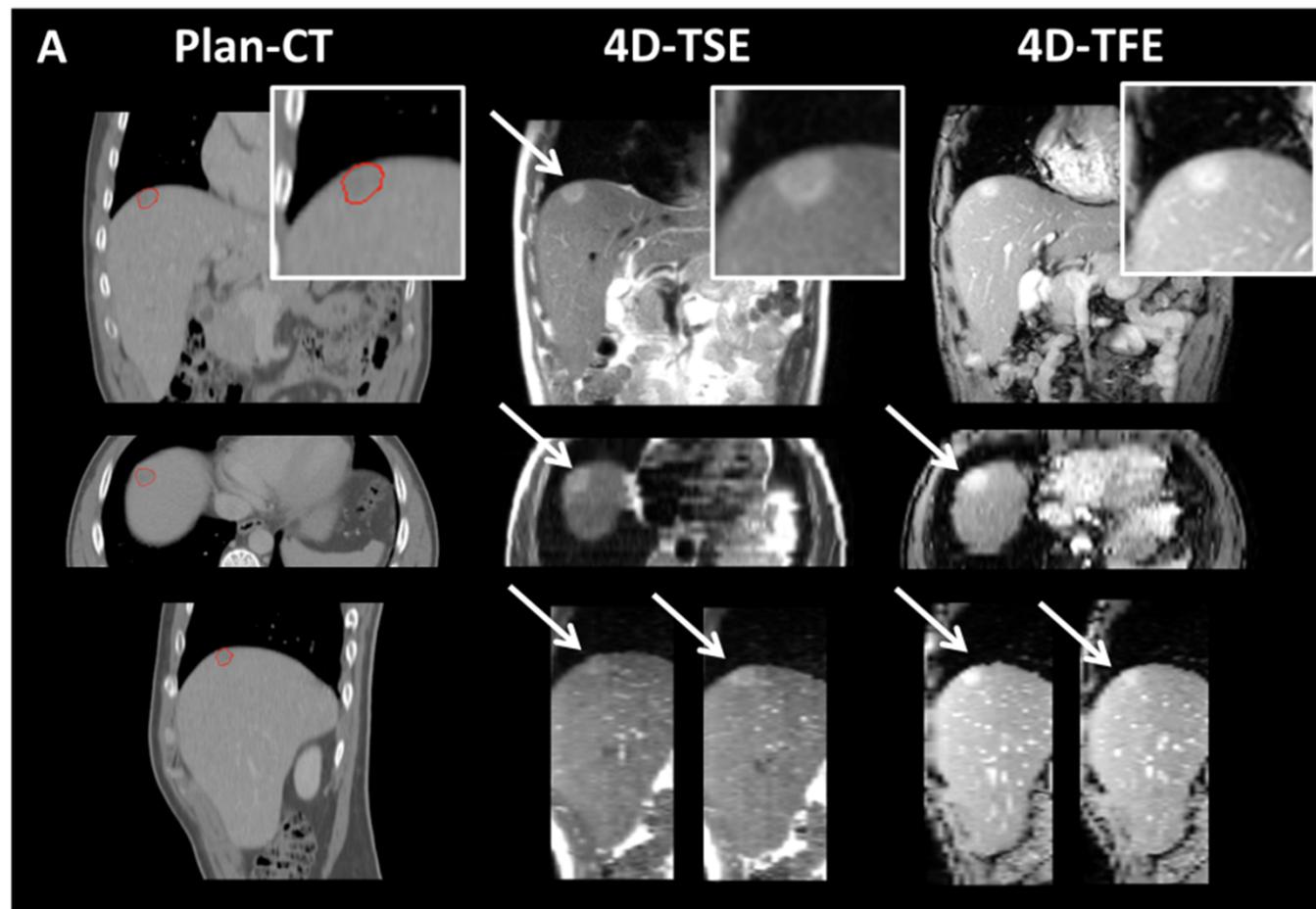
ImS vs NavS		
Correlation	0.95 – 0.97	(range)
RMSD (mm)	1.39 – 2.13	(range)
Time difference inhale positons (s)	$0.06 \pm 0.13$	(mean $\pm$ SD)
Bin difference for amplitude-binning	$0.41 \pm 0.64$	(mean $\pm$ SD)
Bin difference for phase-binning	$0.23 \pm 0.47$	(mean $\pm$ SD)

## RESULTS: AMPLITUDE VS PHASE SORTING



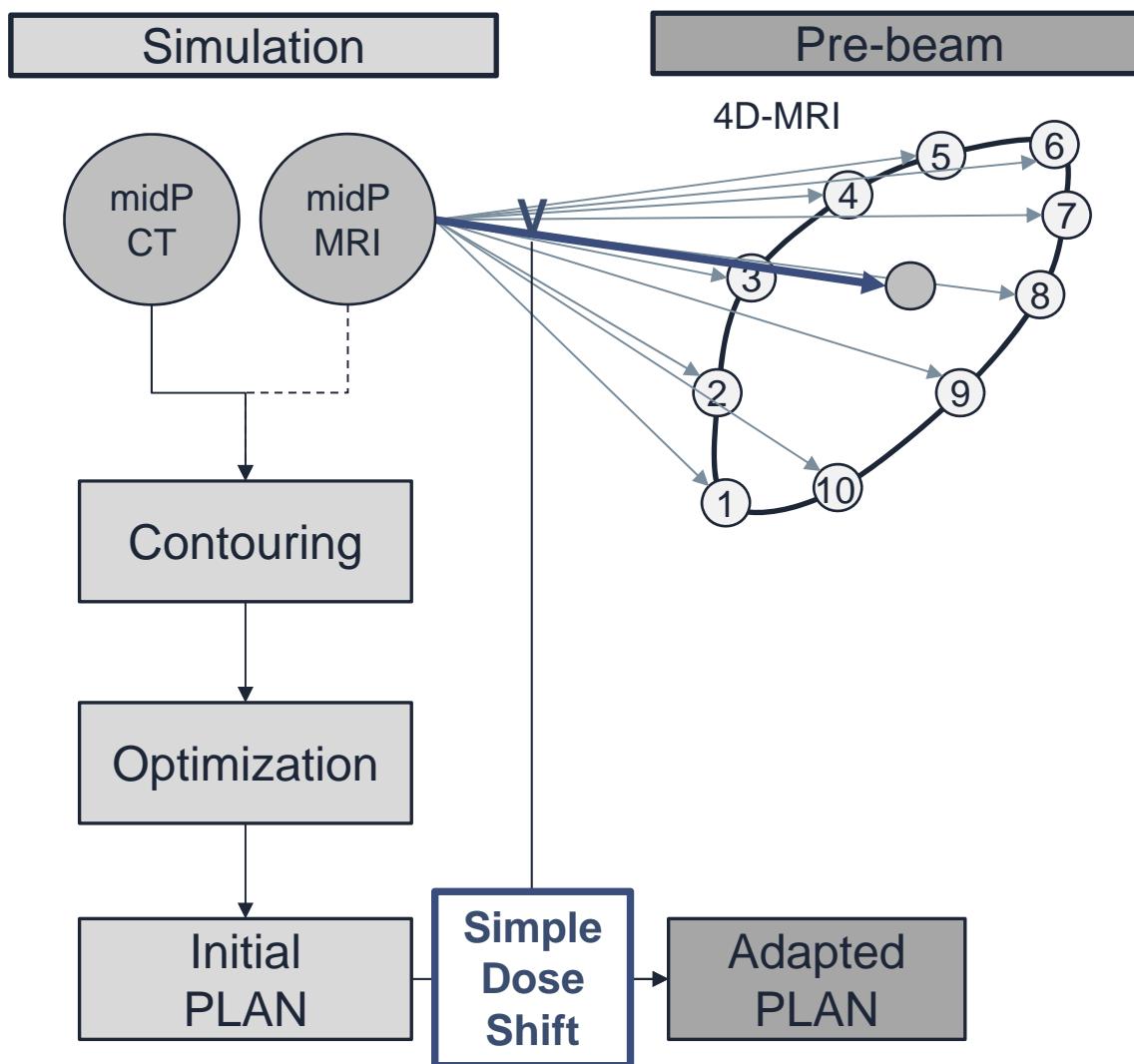
## RESULTS: TUMOR VISIBILITY

Lesion: 15mm



van de Lindt et al (2018), IJROBP

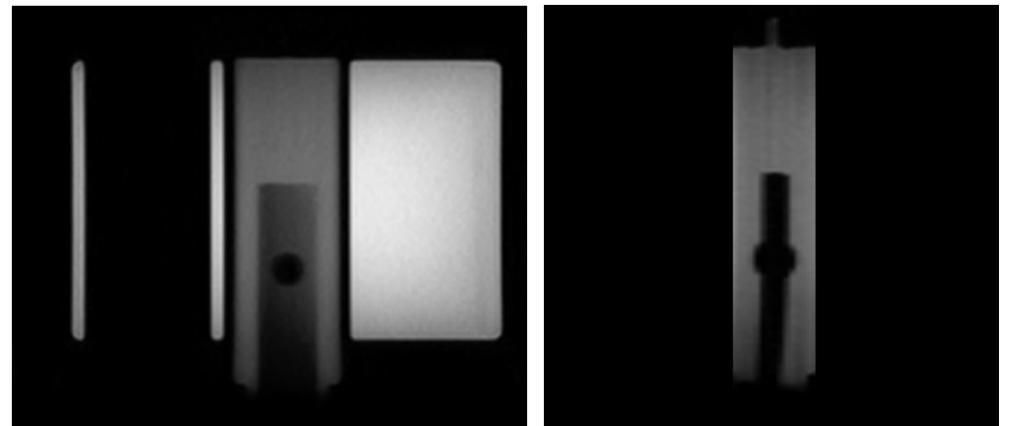
# MR-LINAC: DAILY PLAN ADAPTATION IS A MUST



# MATERIALS & METHODS: EXPERIMENTAL VALIDATION

## 4D-MRI<sup>1</sup>

- Unity MR-Linac
- Coronal multi-2D TSE



## TREATMENT PLANNING

- Monaco v5.19
- 10-beam step-and-shoot IMRT
- 3x20 Gy



## PHANTOM MOTION

- Periodic CC motion
  - A = 15 mm
  - T=4 s
- CC baseline shifts
  - 0, 5, 10 and 15 mm

<sup>1</sup> TN van de Lindt et al., IJROBP., 2018

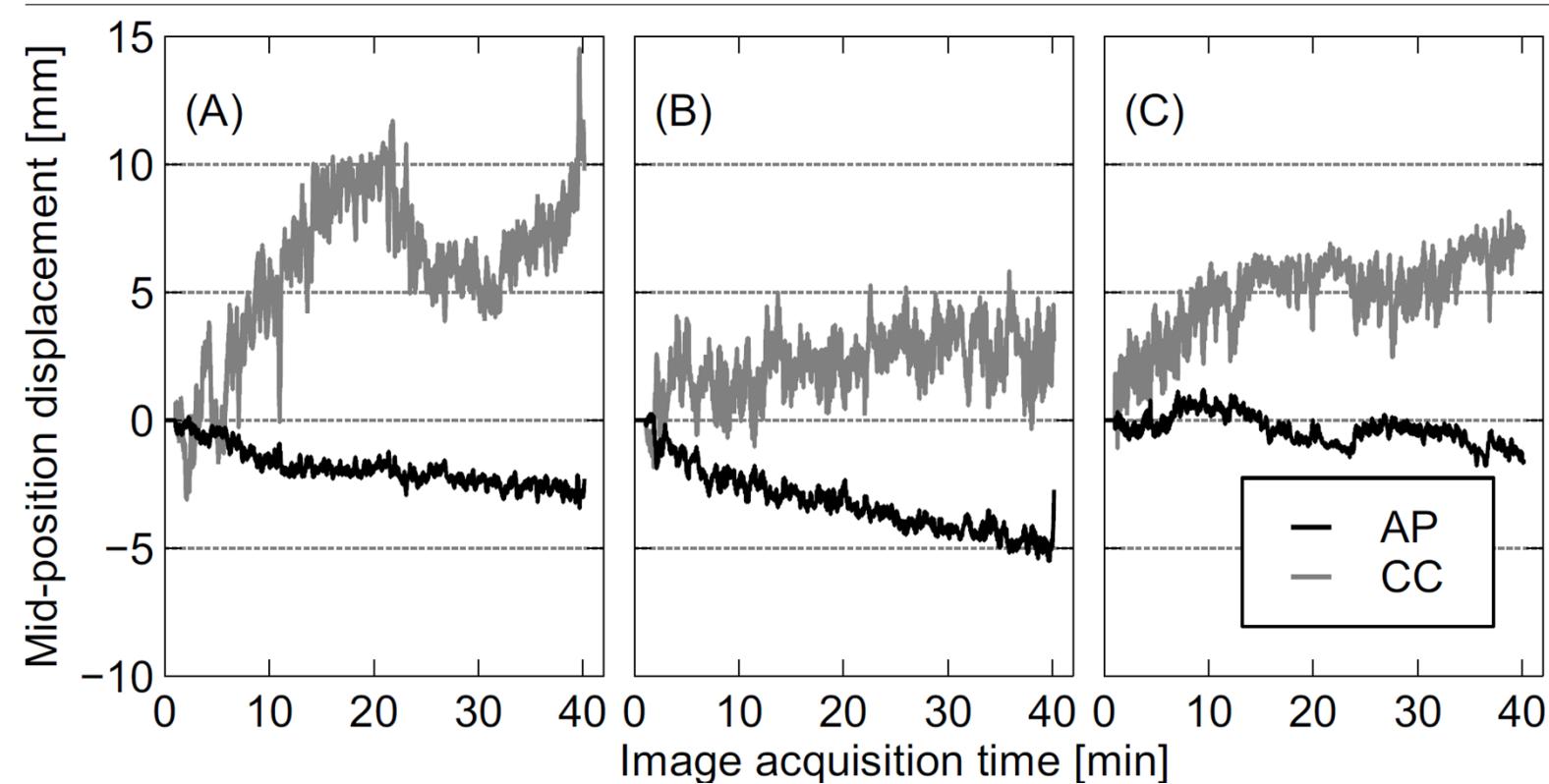
# RESULTS

## GEOMETRIC AND DOSIMETRIC RESULTS

	EPID		MRI	Film	
Baseline shift (mm)	MidP (mm)	Cine (mm)	4D (mm)	Residual CC- shift (mm)	$\gamma$ pass rate (%)
5	5.0	5.3	3.8	1.6 – 1.8	86 – 91
10	9.8	10.6	10.0	0.2 – 0.8	97 – 99
15	15.0	15.5	14.3	-0.1 – 0.8	93 – 99
$\Delta$ Mean $\pm$ SD	0.1 $\pm$ 0.1	-0.5 $\pm$ 0.1	0.6 $\pm$ 0.6	0.8 $\pm$ 0.8	94 $\pm$ 5

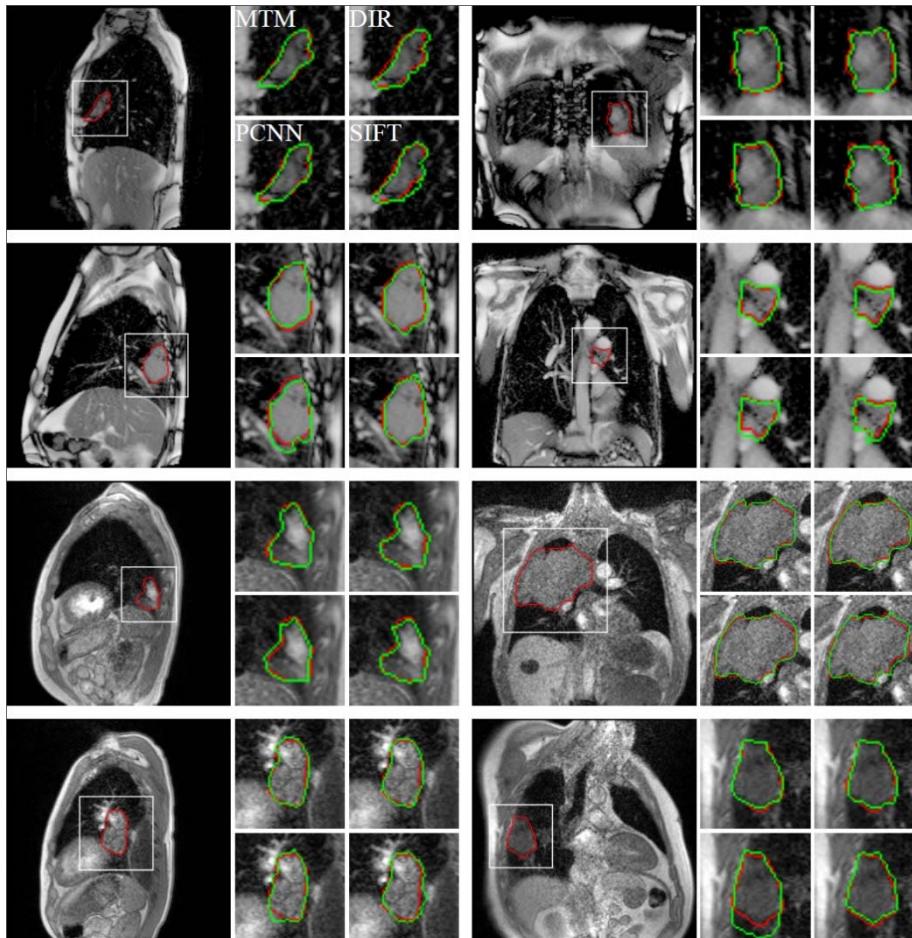
Gamma analysis: 3%/2mm

## NEXT FRONTIER: REAL-TIME ADAPTATIONS



Motion variability not captured by 4d imaging

# CINE MRI + AUTO-CONTOURING



- 6 patients
- 22 image series:  
sequence (bSSFE vs GRE) + image orientation
- Dice: 0.92 (median)
- Centroid distance: 1.5 mm (median)
- Multi-template matching (MTM) and deformable image registration (DIR) performed best

Fast & Eiben et al (2017), R&O

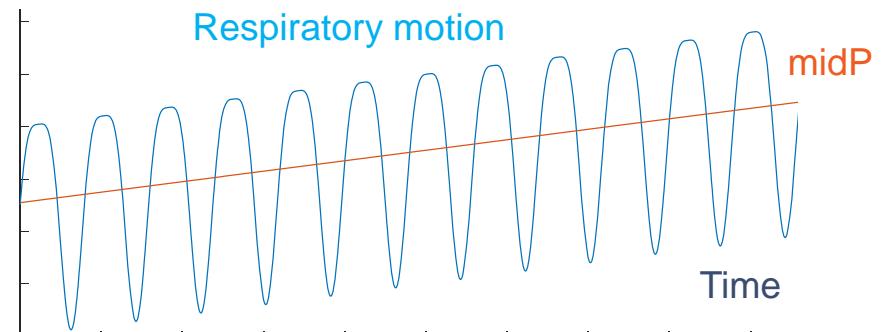
# TUMOUR TRAILING

## REGULAR MOTION

- High-frequency motion components
- Accounted for in mid-position planning strategy

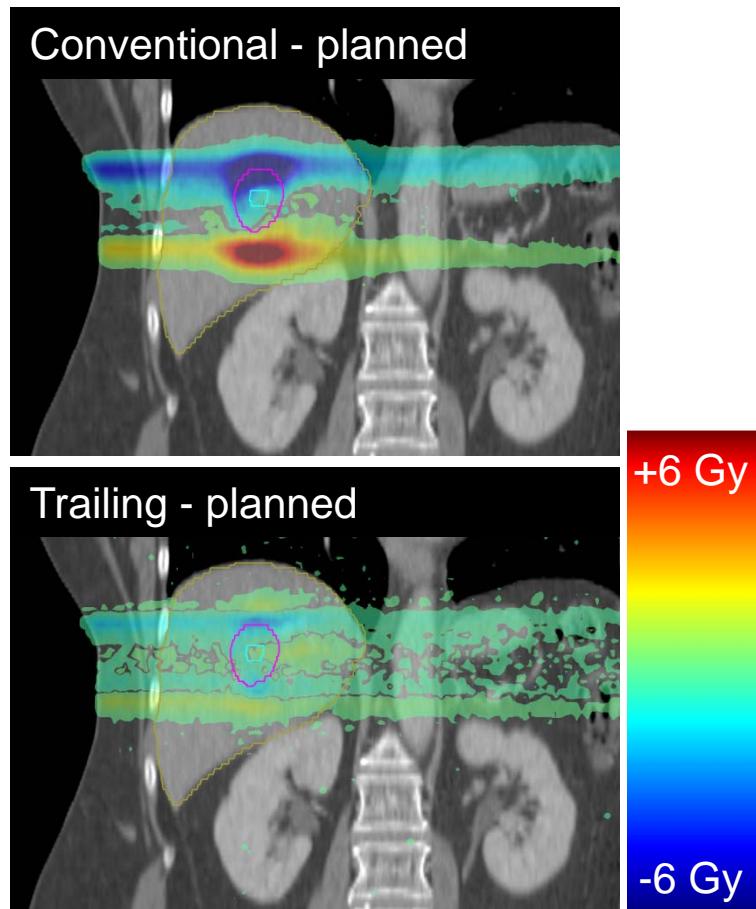
## IRREGULAR MOTION

- Low frequency motion components (slow baseline drifts)
- Following mid-position changes during treatment → Tumour trailing<sup>#</sup>



<sup>#</sup>Trofimov et al (2008), Med. Phys. 35 / George et al (2008), Med. Phys. 35

# MR-LINAC: FEASIBILITY OF TRAILING



- 3x20 Gy liver SBRT
- Simulated delivery to midP CT (full consideration of interplay)
- Baseline drift: 0.5 mm/min (CC) & 0.25 mm/min (AP)
- *Isocentre-shift<sup>‡</sup>* dose reconstruction
- Trailing vs Conventional vs Planned

<sup>‡</sup>Poulsen et al (2012), Med. Phys. / Fast et al (2018), IJROBP

# MR-LINAC: TRAILING PROOF-OF-PRINCIPLE

## Motion monitoring

- Sagittal b-FFE cine-MRI
- $1 \times 1 \times 10 \text{ mm}^3$
- 3 Hz

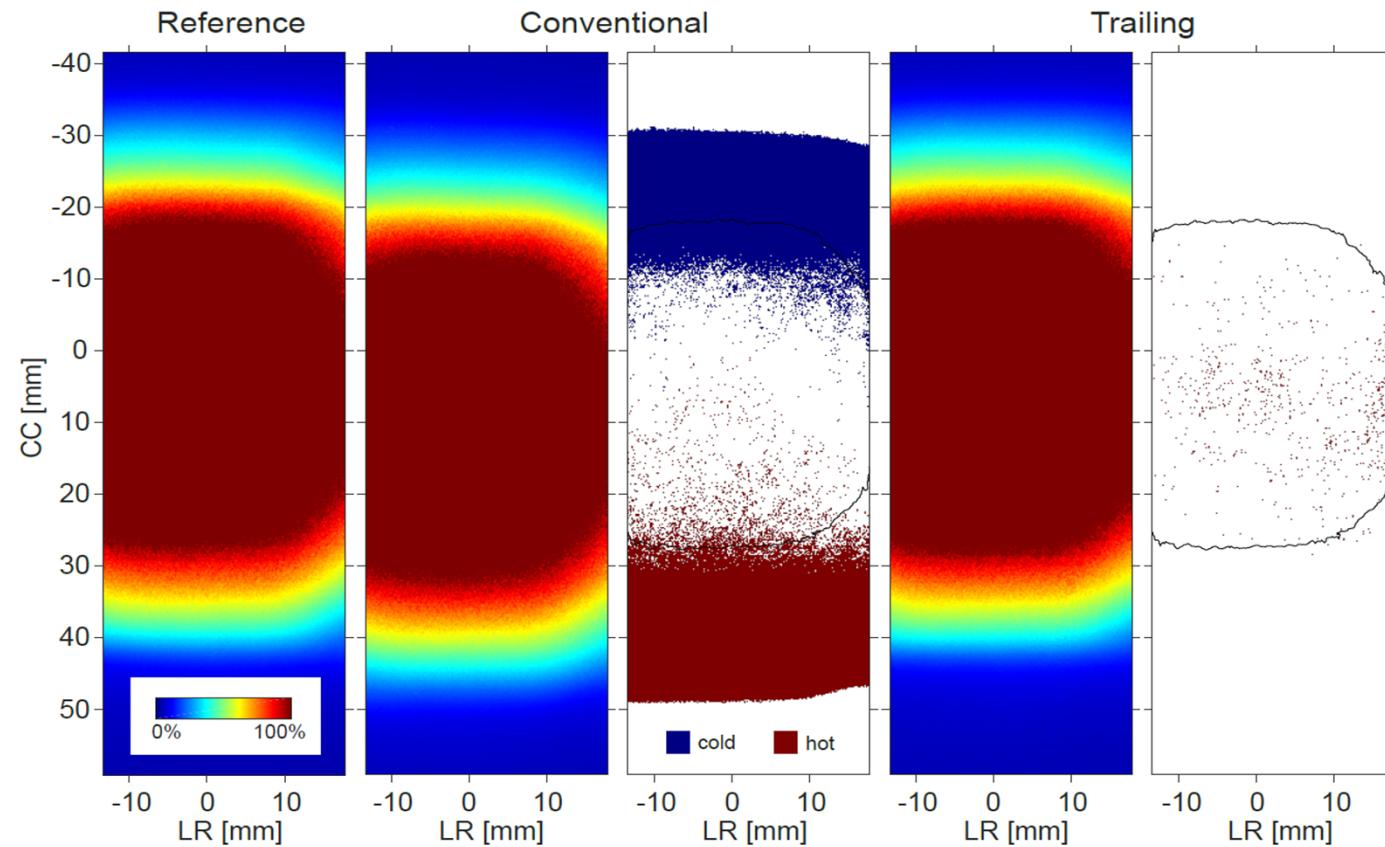
## Plan adaptation

- Triggers for motion  $\geq 1 \text{ mm}$
- Adapts MLC to target in beam's-eye-view

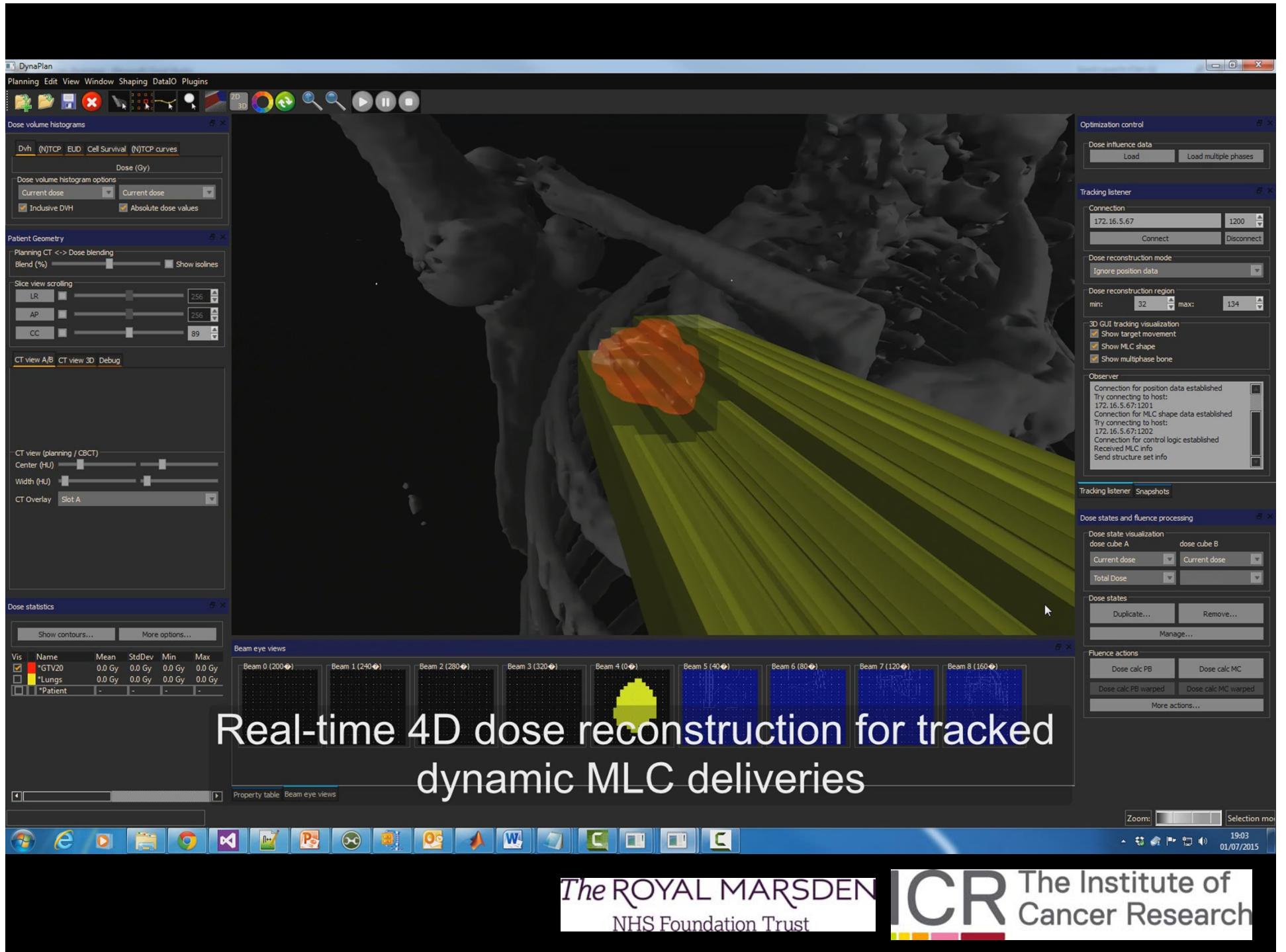
## Trailing

- Starts with initial plan
- Pauses linac when needed
- Transfers adapted plan via iCom interface

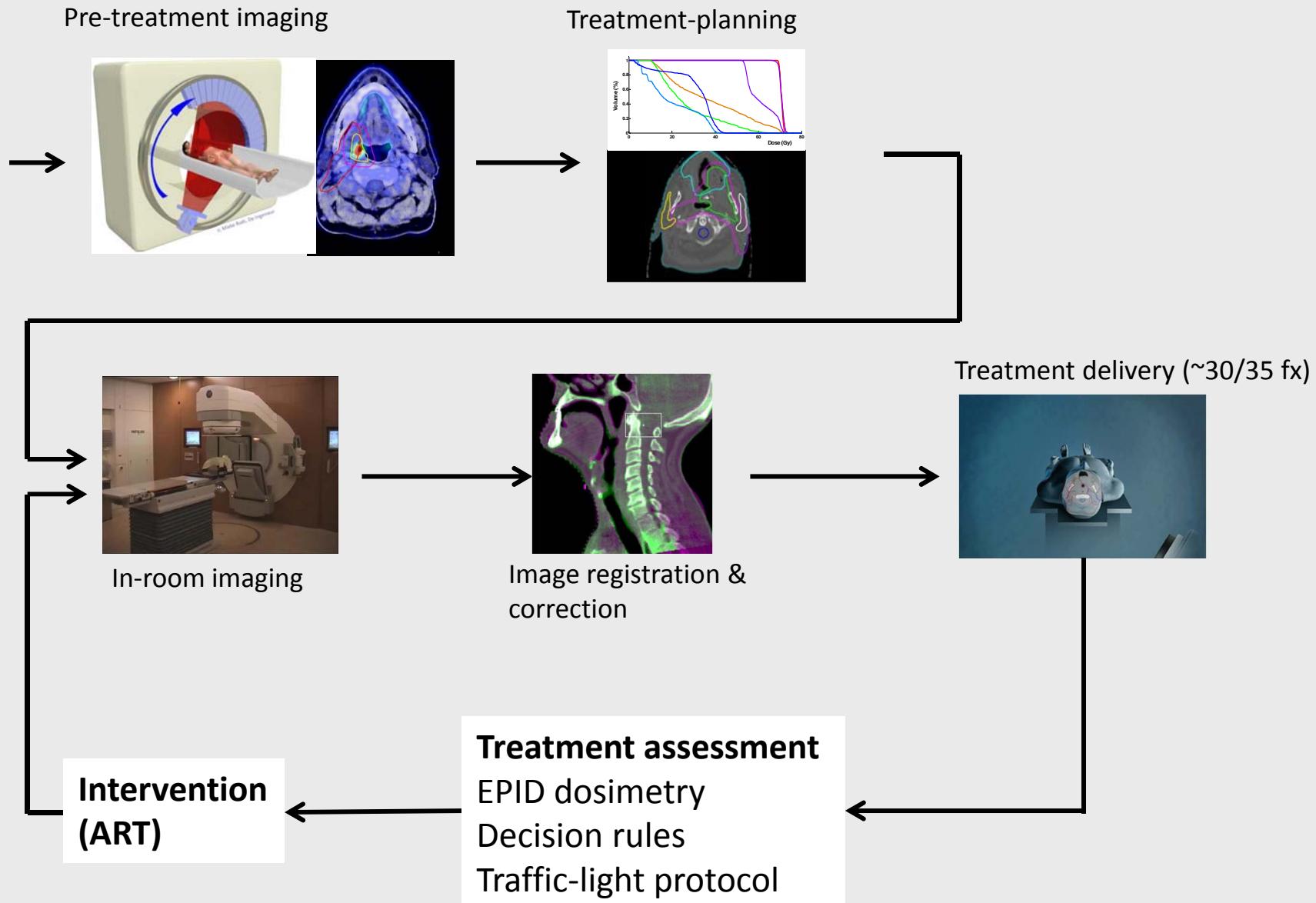
# RESULTS: DOSE AND GAMMA-DISTRIBUTION



Gamma analysis: 3%/2mm



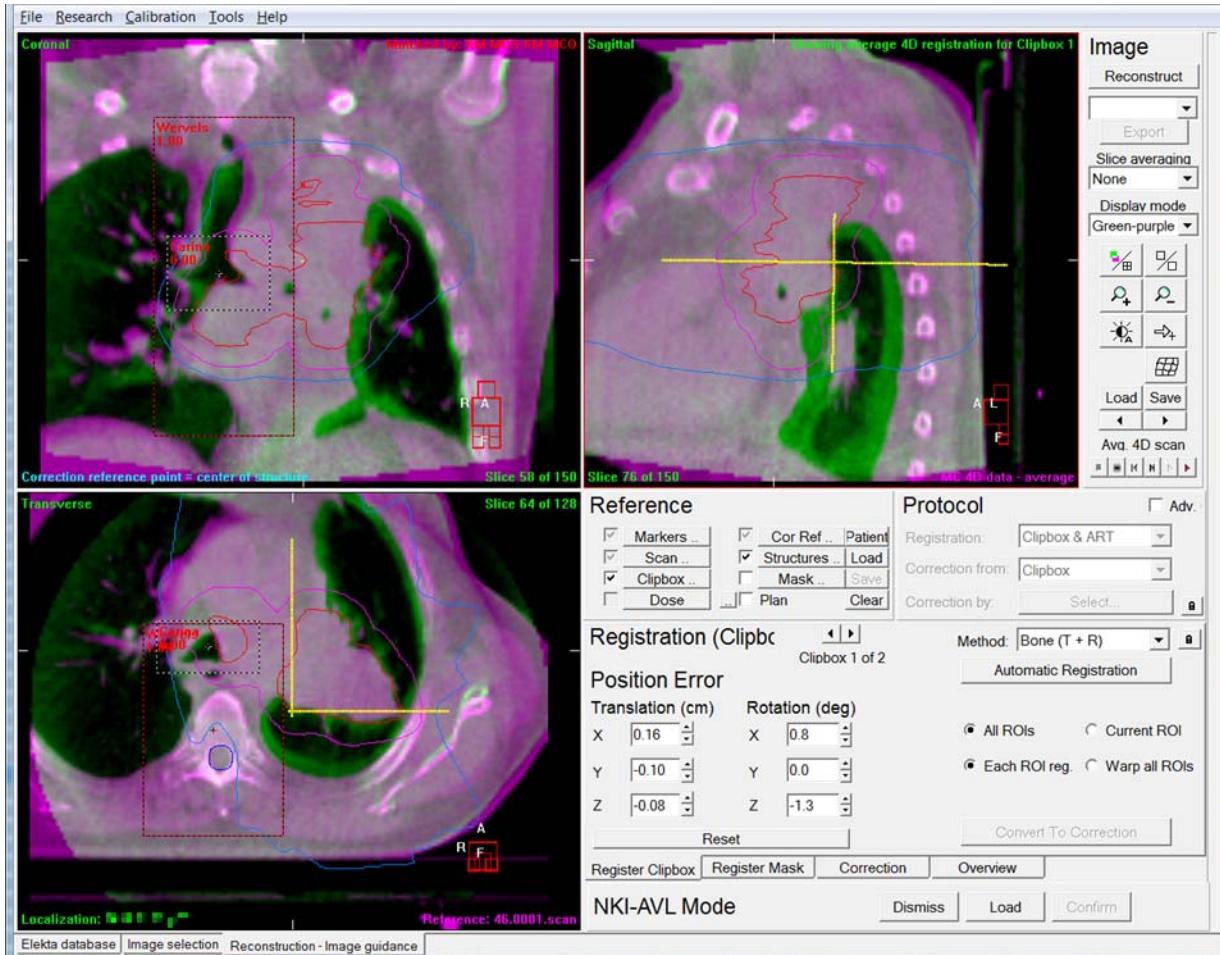
# The (adaptive) Radiotherapy Process



# Introduction – current practice

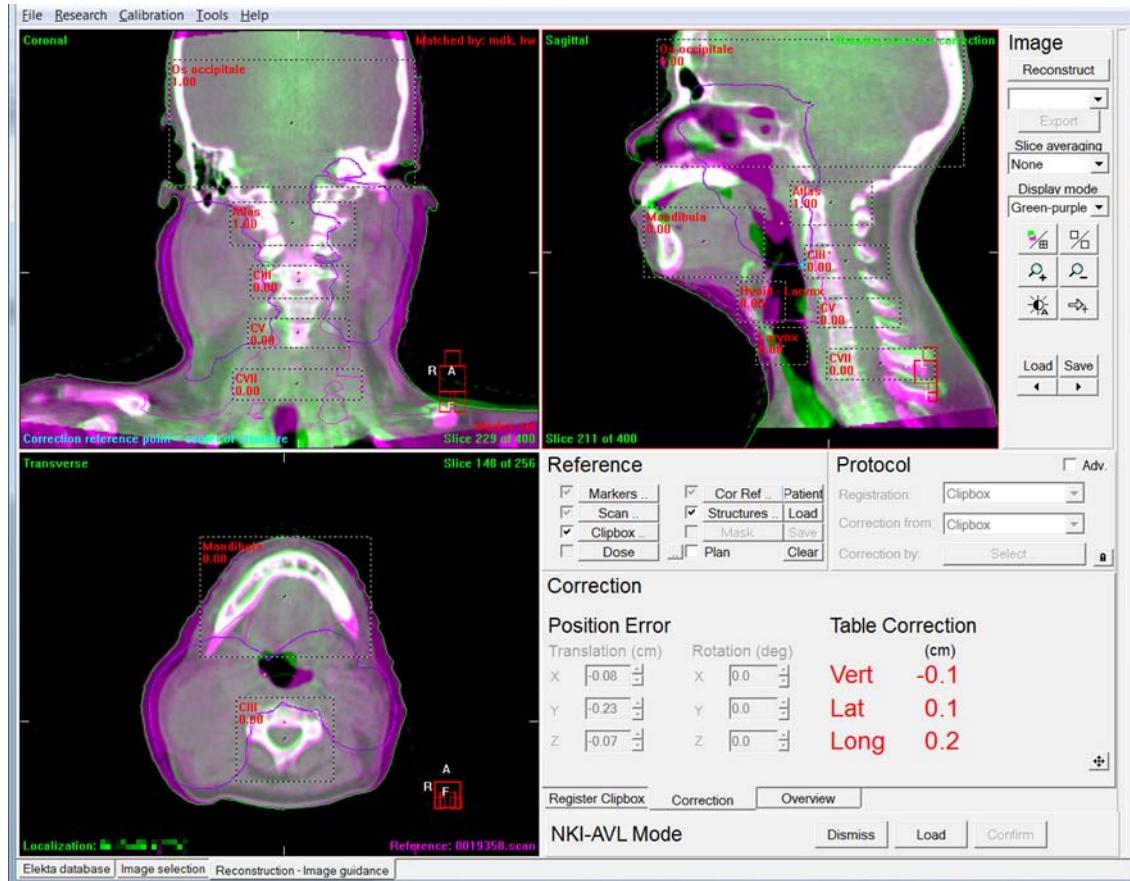
- EPID: *traffic-light* for dose differences with planned  
>> but what does it mean in the anatomy?
- IGRT: Decision rules & *traffic-light* protocol  
>> we see deformations, what does it mean?
  - Dual registration Lung
  - Multi-clipbox HNC
- Ad hoc assessment: editing the pCT for weightloss/deformations in Pinnacle ...

# Example lung



- Lung Cancer
- 60 Gy, 30 fxs
- Previously irradiated:  
cord dose < 20 Gy
- NTD (a/b=2)

# Example HNC



- Nasopharynx
- SIB 70 Gy, 35 fxs
- Large PTV
- Many OARs:  
N. Opticus, Chiasm,  
Brainstem
- mROI with weights  
1/0

# What these examples show

Mental exercise...

- Isodose lines: is that what we delivered?
- Deformations: how does that change CTV/OAR dose?
- History: Systematic? Random? Trend?
- Timing: How much can we still gain with replanning?
- Upon replanning: what about dose already delivered?

→ We see geometry, we must think dose...

>> HEADACHE!



# Alternative: dose accumulation

alternative: dose accumulation

*compute the total delivered dose  
in the patient while accounting for  
dosimetric and geometrical discrepancies*



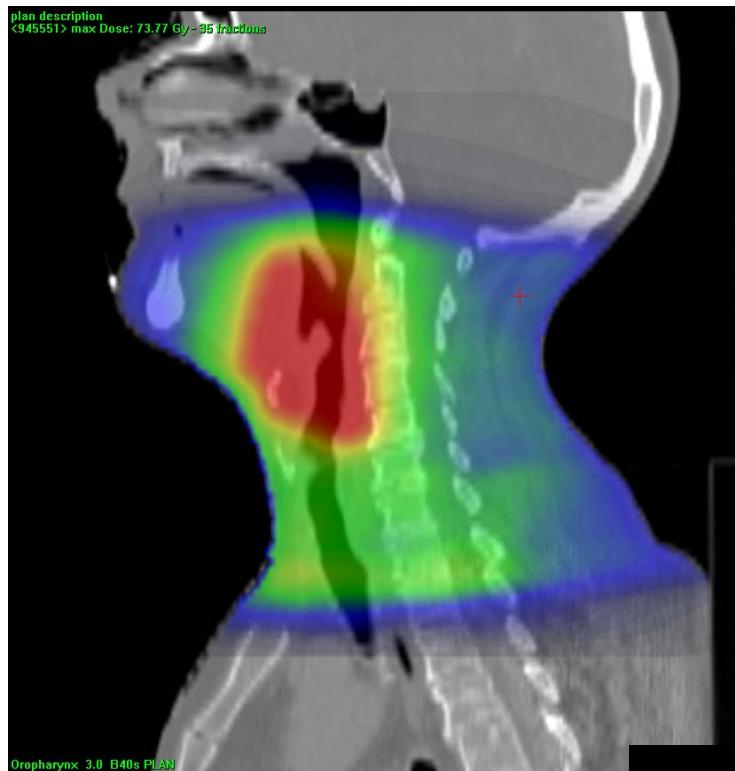
2 important steps:

- Dose distribution delivered is different than planned
- Dose ends up at different location than planned

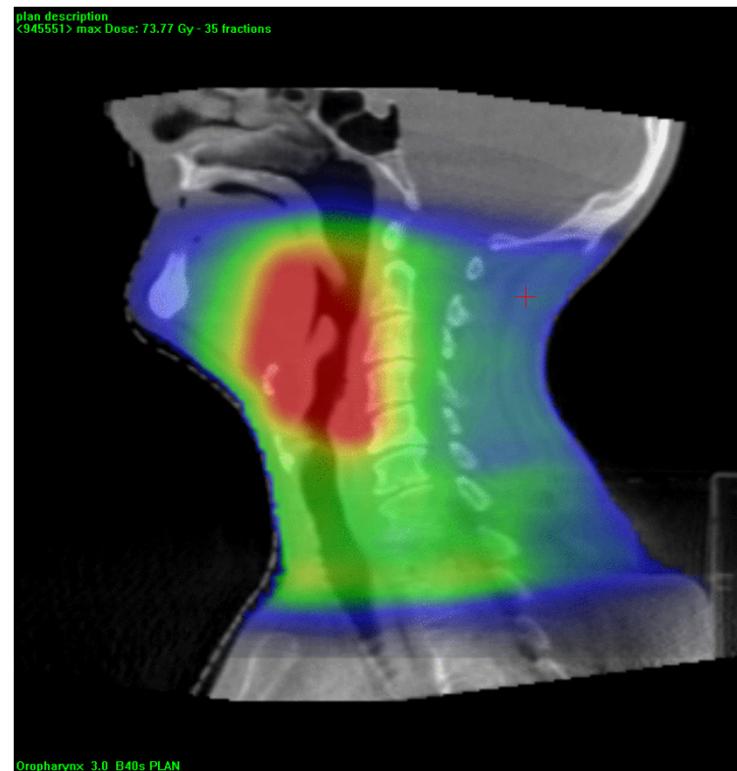


# Dose accumulation

Step 1: Dose distribution delivered is different than planned



Planned dose in pCT



planned/recalculated dose in CBCT

# Dose accumulation

Step 2: Dose ends up at different location than planned



Deformation & anatomy  
differences



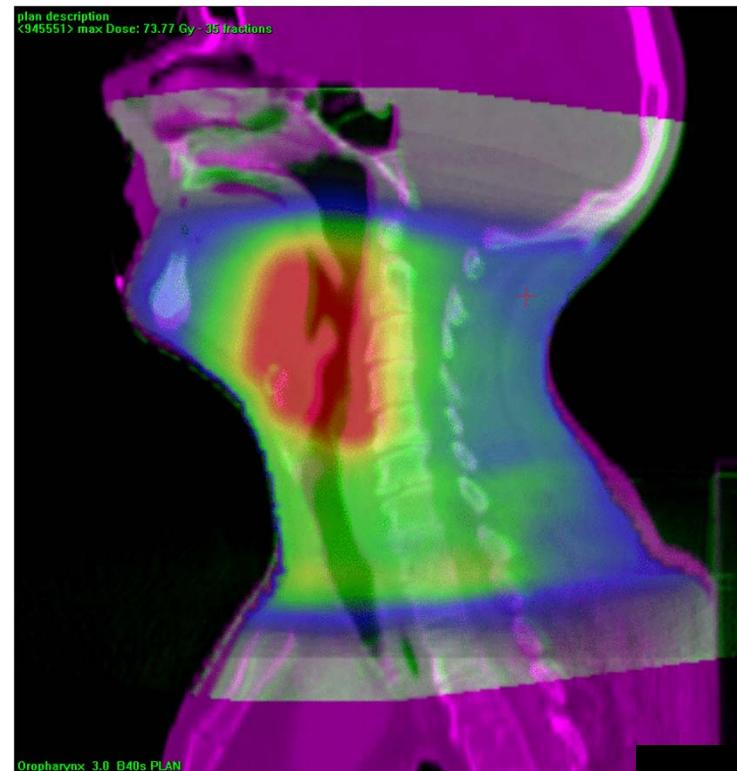
CBCT warping

# Dose accumulation

Step 2: Dose ends up at different location than planned



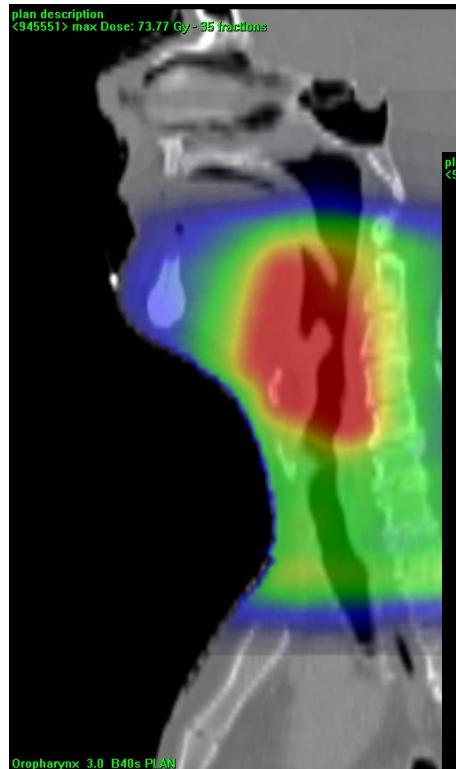
Deformation & anatomy  
differences



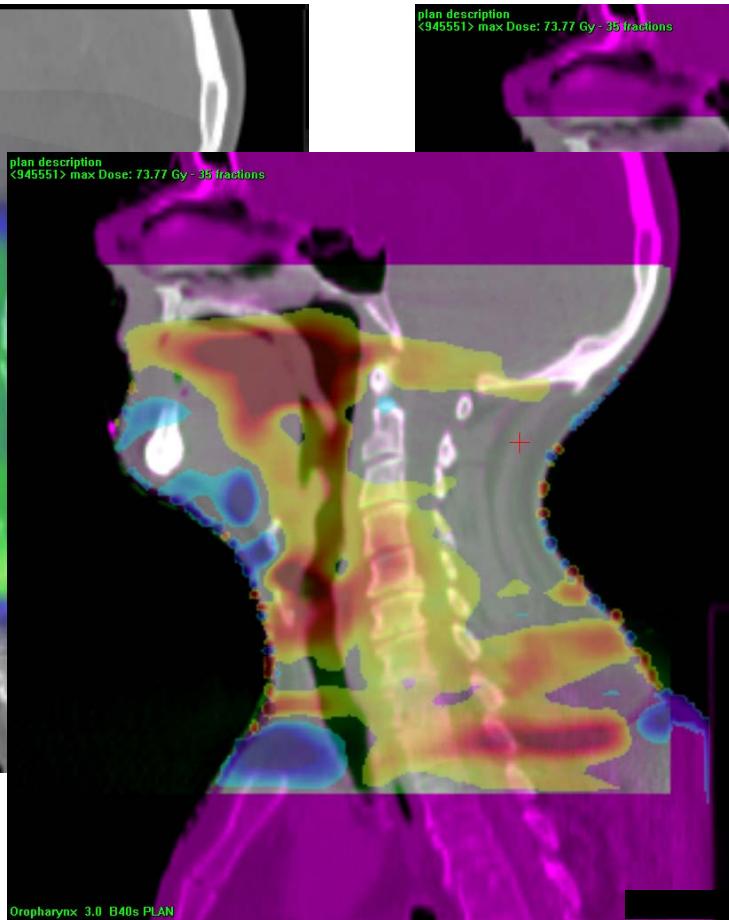
dose warping

# Dose accumulation

After dose warping: common reference



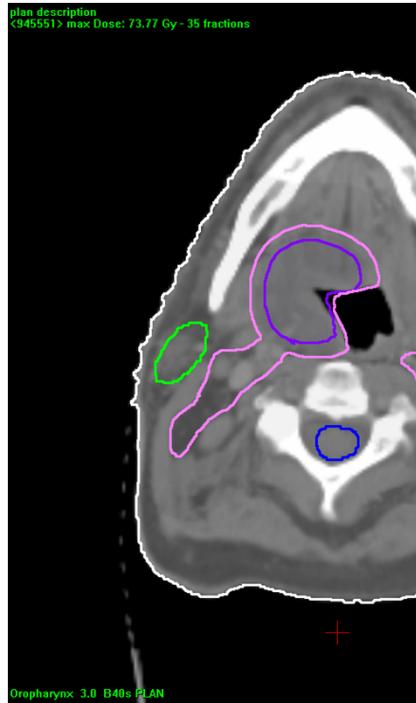
planned dose



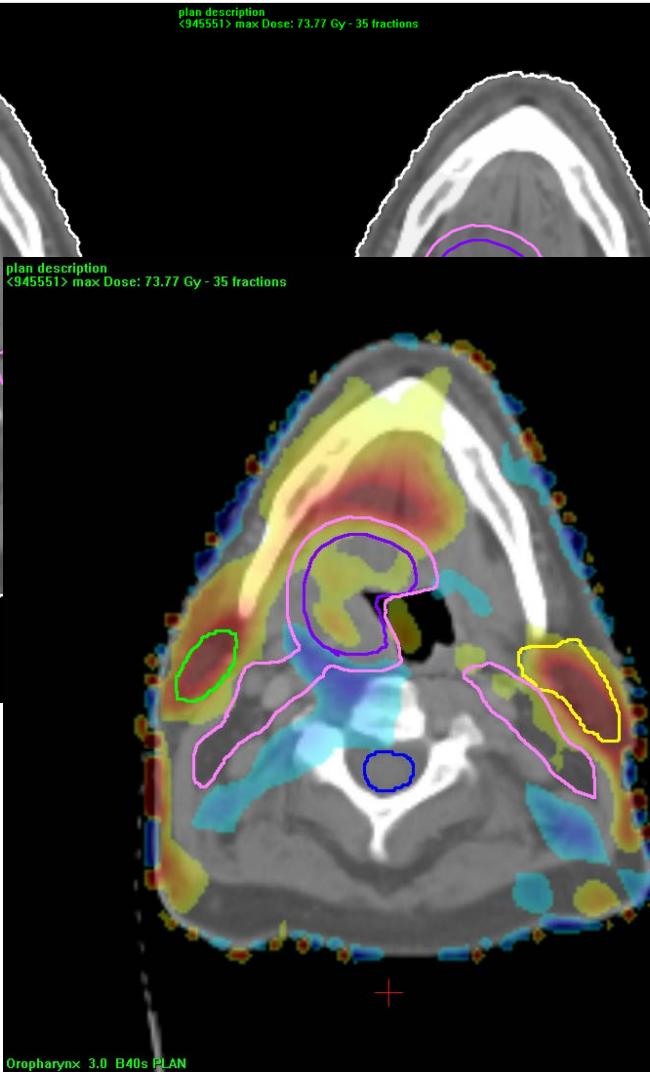
warped dose

# Dose accumulation

Planned dose



Accumulated dose

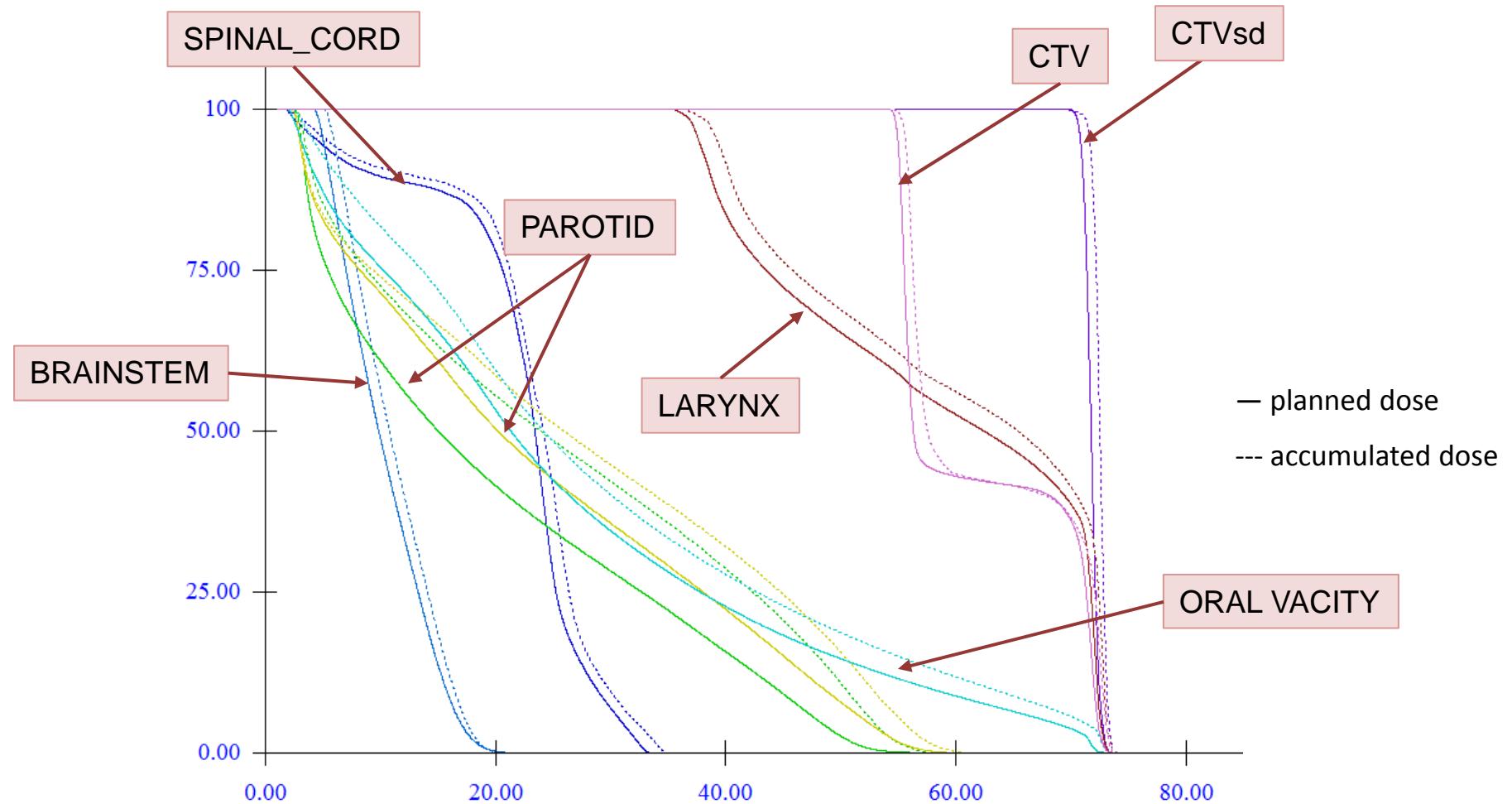


Difference dose

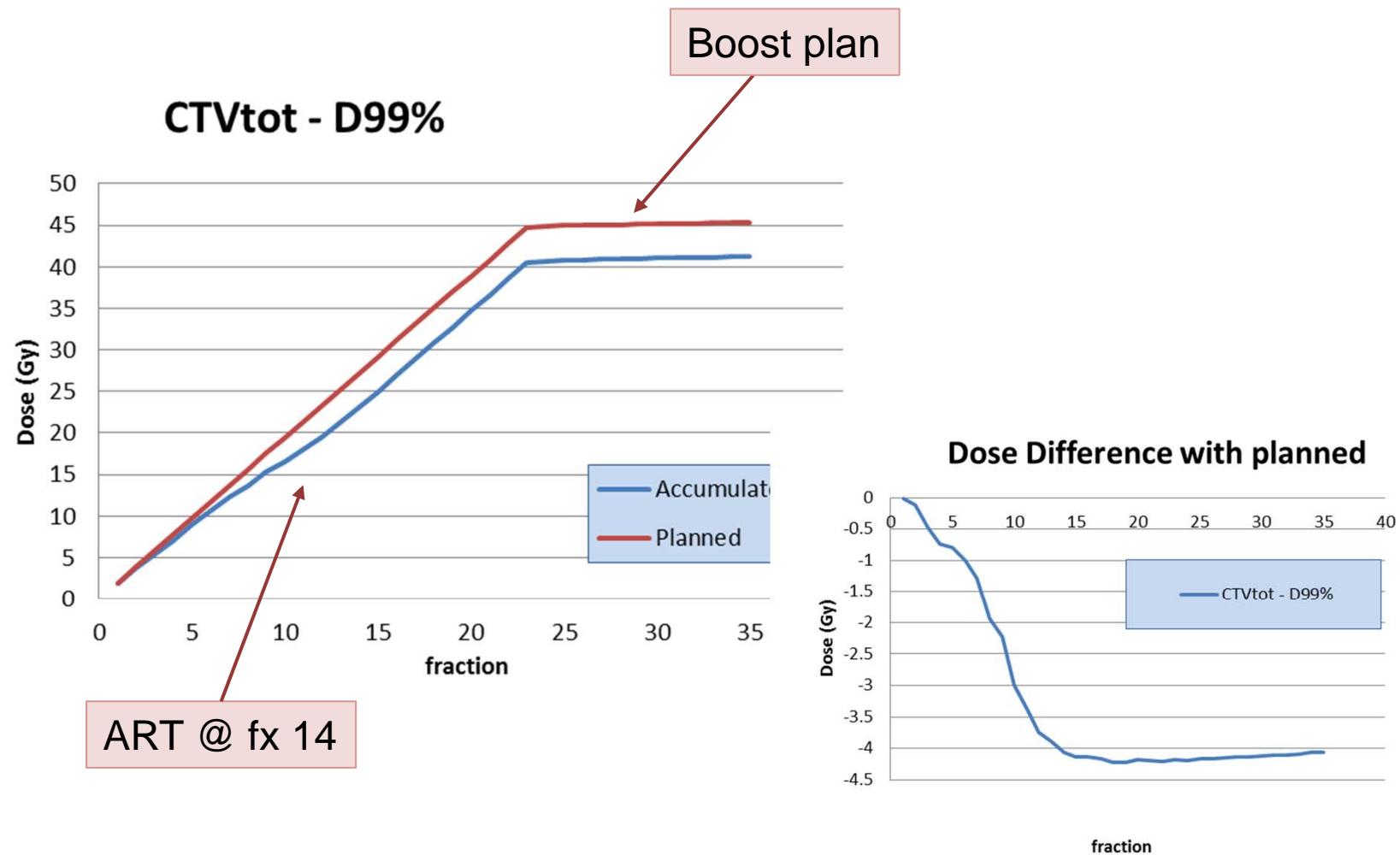


# Dose accumulation: DVH differences

DVH: accumulated dose vs planned dose



# Challenges: prediction of final dose

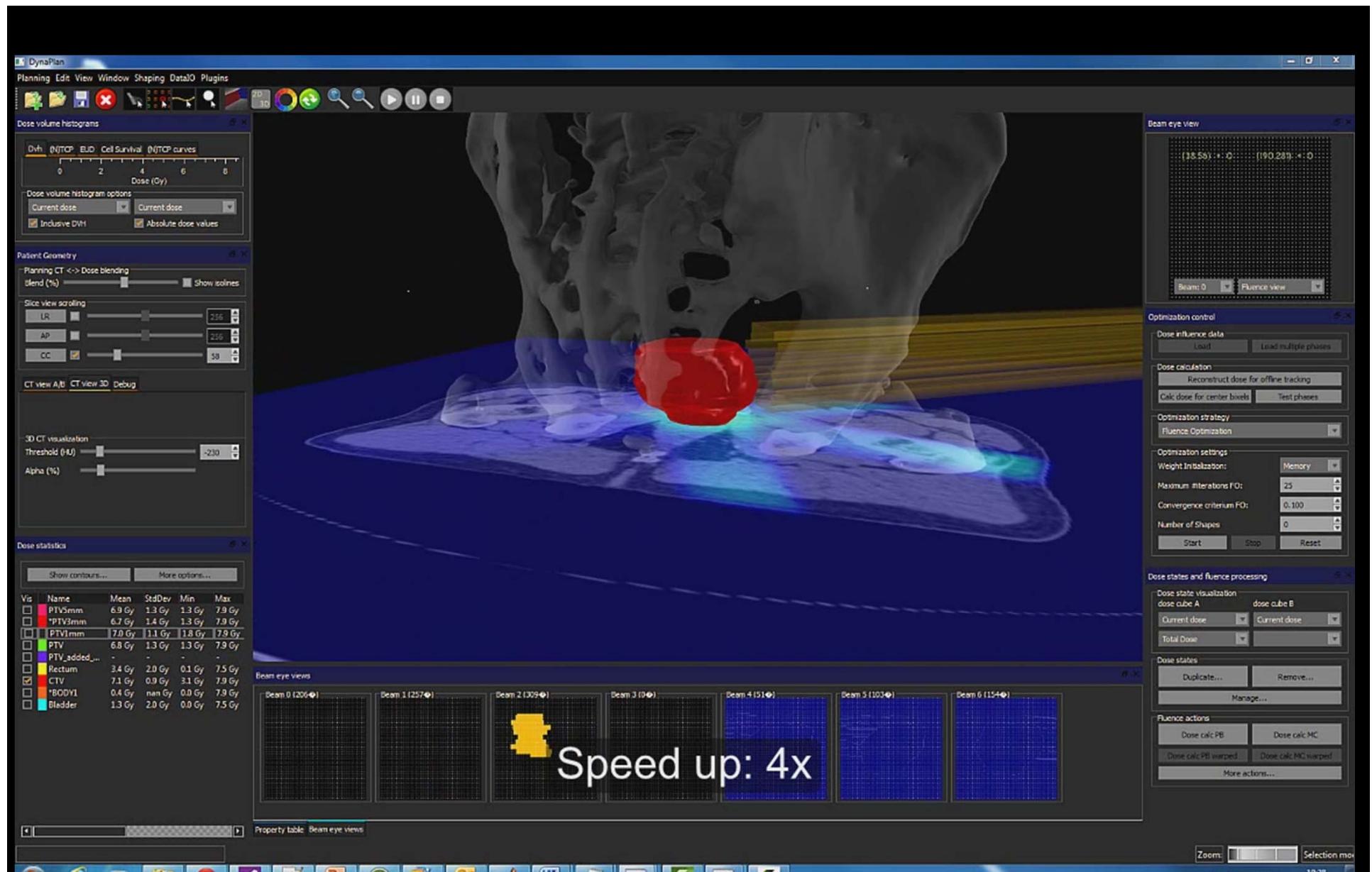


# Challenges: DIR with limited Image Quality

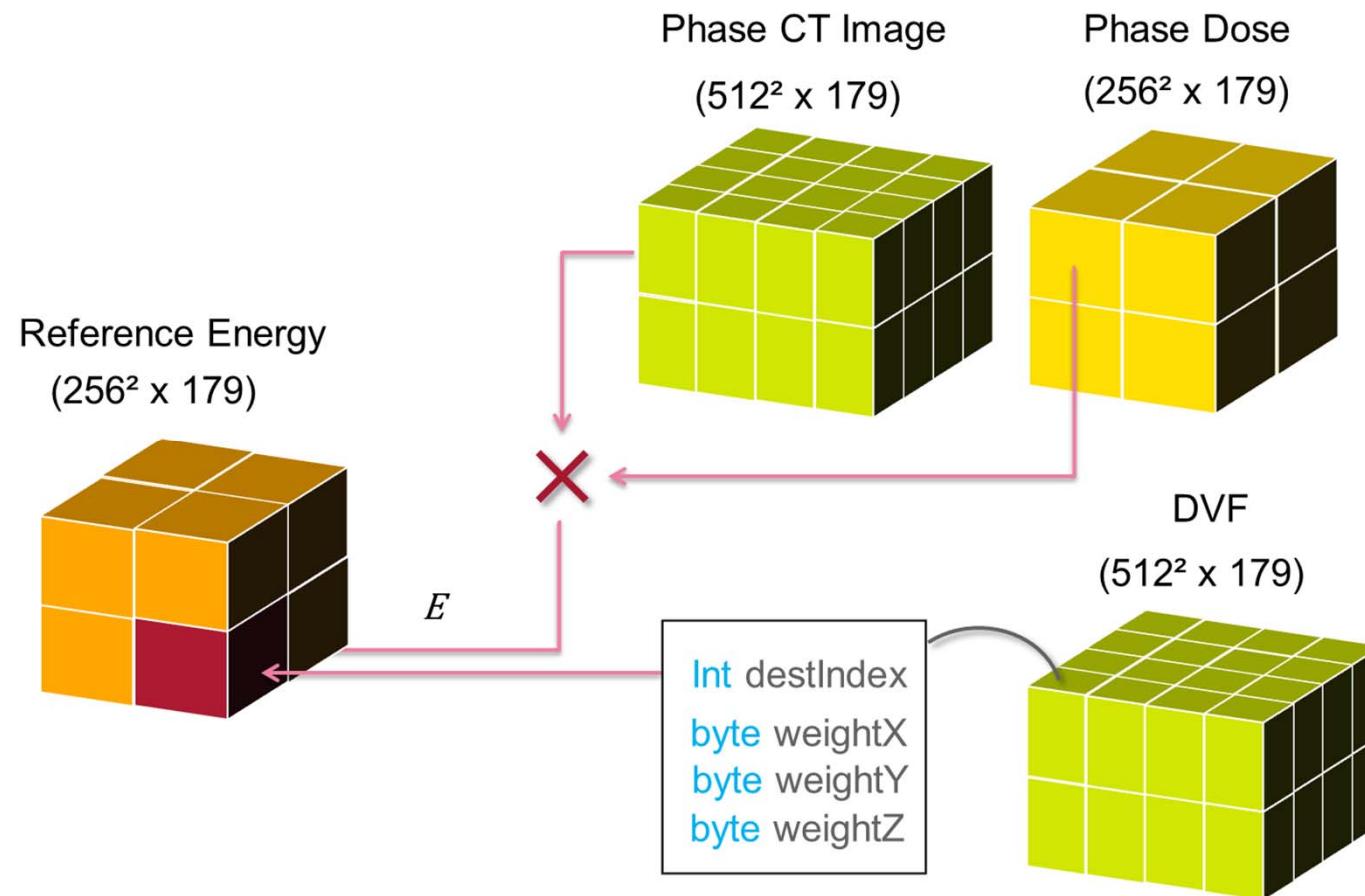
- HNC: OK...
- Lung: WIP...

Example image quality rectum





# DOSE ACCUMULATION: ENERGY-MASS TRANSFER



Li et al. (2014), Med. Phys. / Ziegenhein et al (2018), Sci. Rep.

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## SUMMARY & OUTLOOK

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- MRI-guidance provides excellent soft-tissue contrast
- Novel 4D-MRI radiotherapy solutions are being developed
- Margin reduction / active motion management will provide scope to allow for re-irradiations
- Away with the surrogate reality: start looking at dose in anatomy daily