



# Determining the dose outside the treatment field

**Stephen F. Kry, PhD**

**Workshop on Risk of secondary cancer following  
radiotherapy**

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THE UNIVERSITY OF TEXAS  
**MDAnderson  
Cancer Center**

Making Cancer History®

# How do we determine stray radiation dose?

## 1. Dose assessment

1. *Treatment planning system*

2. *Measurement*

3. *Neutrons*

4. *Monte Carlo*

## 2. Dosimetric assessment for radiation epidemiology studies

1. *Individual dosimetry*

2. *Reference cases*

# 1. Dose assessment

- See upcoming AAPM report:

Task Group 158

Measurement and Calculation of Doses Outside the Treatment Volume from External-beam Radiation Therapy

Stephen Kry, Bryan Bednarz, Rebecca Howell, Larry Dauer, David Followill, Eric Klein, Harald Paganetti, Brian Wang, Cheng-Shie Wu, X. George Xu.

- Approved by AAPM, publication pending in *Medical Physics*

# 1.1 TPS accuracy outside the treatment field

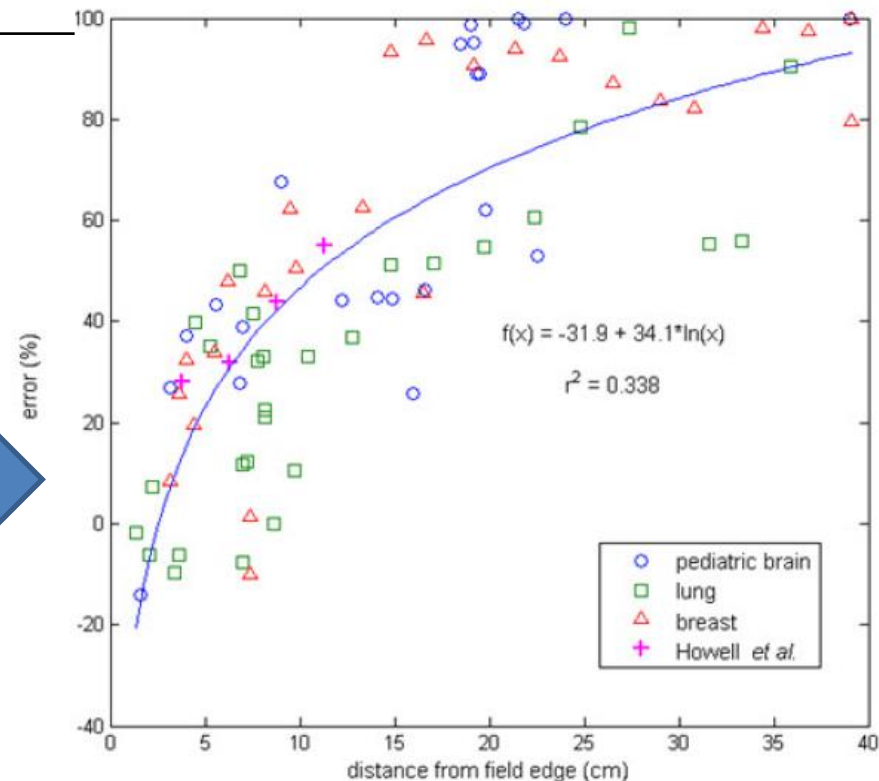
Distance from Field Edge (cm)	$D_{\text{calc}}$ (cGy)		$D_{\text{meas}}$ (cGy)		Percent Difference
3.75	3.08	0.61	4.24	0.45	38%
6.25	2.02	0.43	3.01	0.24	49%
8.75	1.16	0.32	2.09	0.14	80%
11.25	0.66	0.33	1.49	0.13	126%

- Poor accuracy even close to the field
- This is for a simple, conventional field.

Howell et al, 2010

- Not an easier calculation with complex contemporary fields
- Again, poor agreement
- Consistently underestimates dose

Huang et al, 2013



# 1.1 TPS guidelines

- Beyond 3 cm from field edge  
or
- Below 5% isodose line
  
- Don't expect the TPS to give you the right answer

# 1.2 Out-of-field Photon Measurements

- 4 general measurement considerations that are particularly relevant to out-of-field measurements:
  1. Dosimeter dynamic range – must be able to get sufficient signal (can be easy with phantom – scale MU)
  2. Dose at the surface,
  3. Energy spectrum,
  4. Presence of other particles.

**For various dosimeters, TG-158 considers specific implications of measurement considerations**

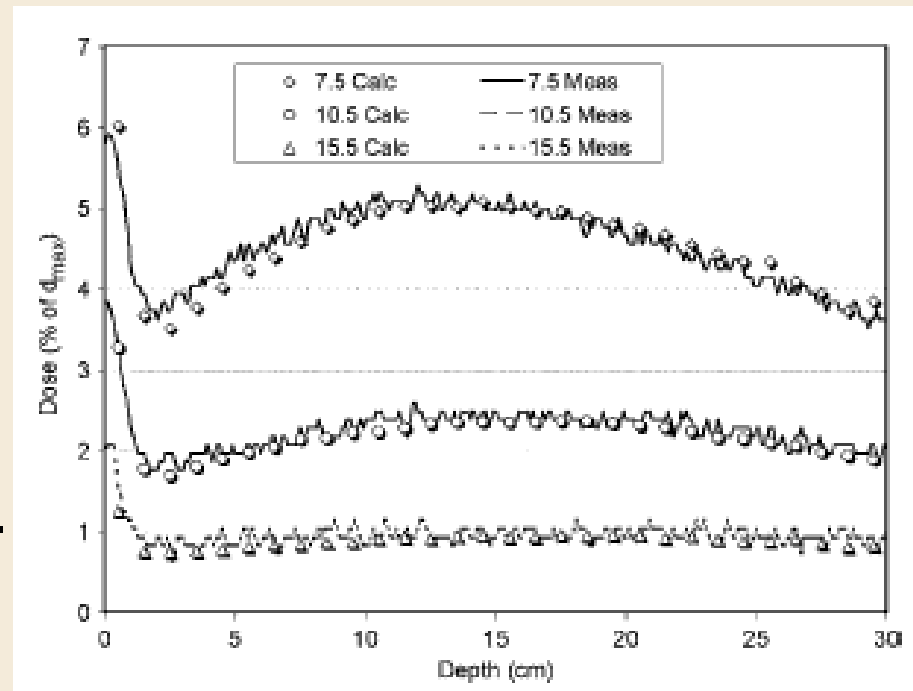
**TLD  
OSLD  
Diode  
MOSFET  
Ion chamber**

# 1.2 Out-of-field Measurements

## Dose at the Surface

- Outside the treatment field, the superficial dose is increased by stray electrons, so there is a build-down effect instead of a build-up effect at the surface.
  - The dose is 2-5x higher at the patient surface, and decreases to  $\sim d_{max}$ , below which the dose becomes  $\sim$  constant with depth.
  - If a dosimeter is placed on the patient surface, it will overestimate the dose (by 2-5x).

- Dosimeter should be covered by bolus of a thickness of  $\sim d_{max}$ .



# 1.2 Out-of-field Measurements

## Energy Spectrum Considerations

- The average beam energy is much lower outside the treatment field. (0.2-0.5 MeV vs 1.5 MeV)
- A dosimeter that is not tissue equivalent will over-respond to this softer radiation relative to its calibration, which will generally be based on the 1° beam.
  - This effect can be sizeable to the point of unacceptable accuracy unless it is accounted for.

### TLD/OSLD

- Overresponse **2-12%/5-30%** compared to in-beam.

### Diode

- Overresponse **up to 70%** compared to in-beam.

### MOSFET

- Overresponse **50 to 600%** compared to in-beam.

### Ion Chamber

- Overresponse **negligible**, compared to in-beam.



# 1.2 Out-of-field Measurements

## Other Particle Considerations

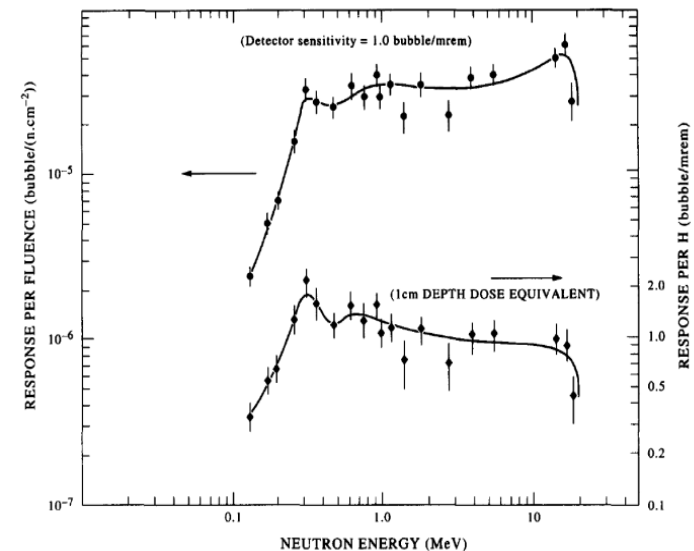
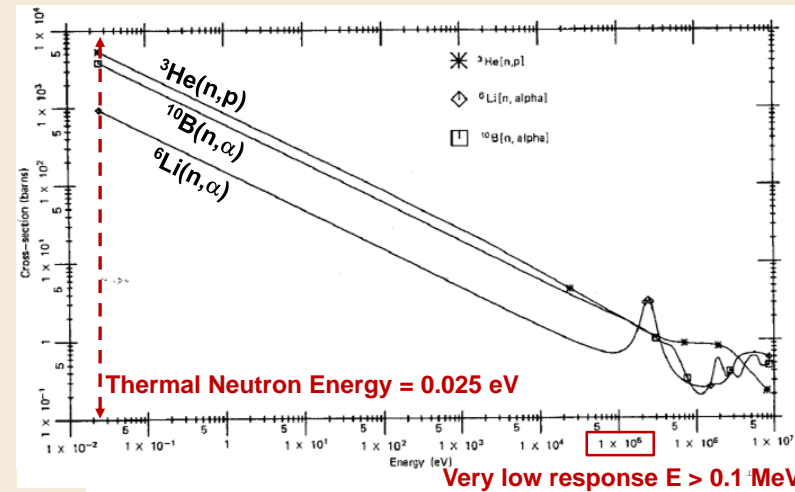
- It is important to know and consider if measurements are being made in a mixed field
  - Dosimeters can respond very differently to different types of radiation.

### **TLD-100: LiF:Mg,Ti**

- The standard TLD-100 overresponds to neutrons by as much as 10-12x (compared to photons).
  - A neutron-insensitive dosimeter (such as TLD-700) should be used to measure photon doses (for >10 MV).
  - separate neutron dosimetry should be conducted to determine the neutron dose.

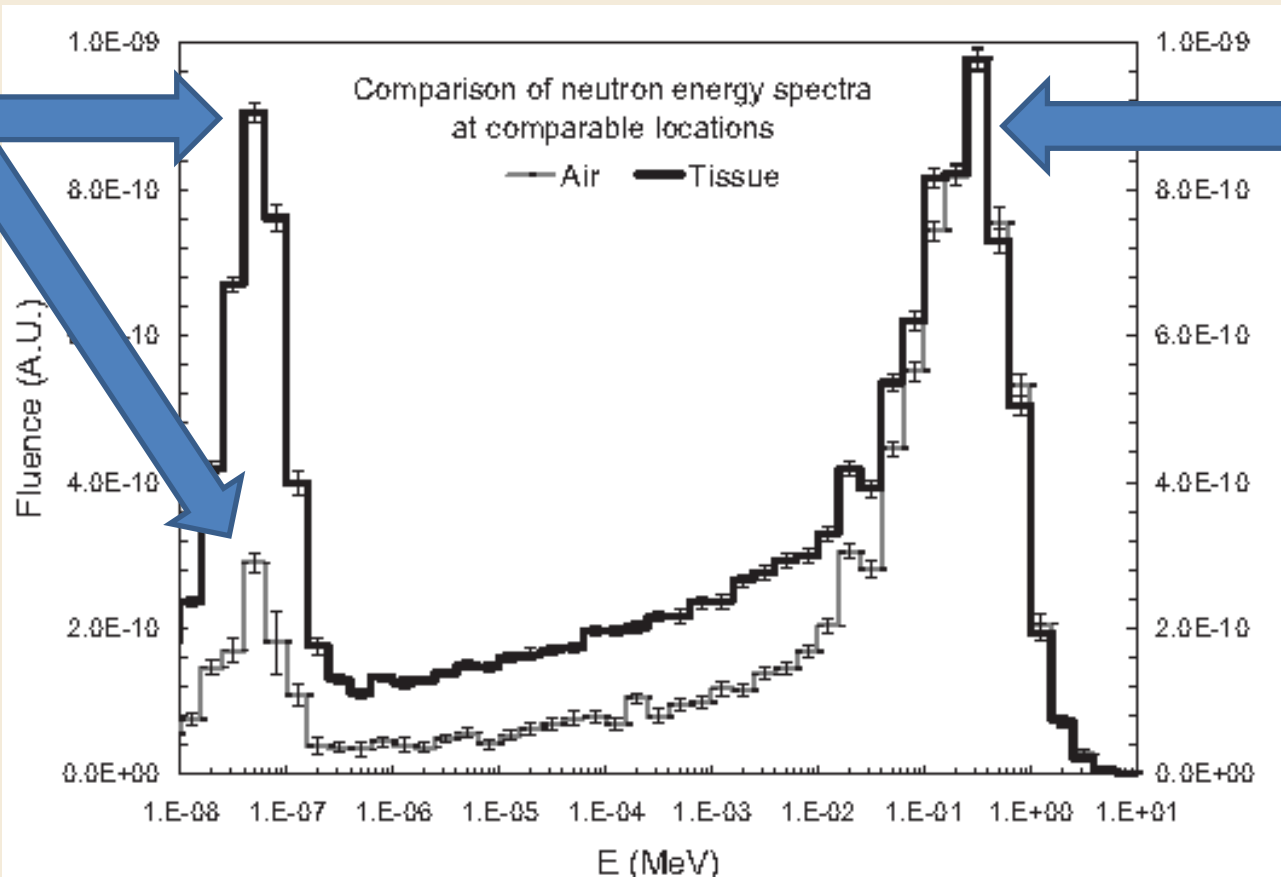
# 1.3 Neutron Dosimetry

- Neutron detectors exhibit strong energy dependence.
- Thermal neutron detectors.
  - Passive detectors, e.g., TLD-600,  $^{197}\text{Au}$  activation foils
  - Active detectors, e.g.,  $^3\text{He}$ ,  $^{10}\text{B}$ ,  $^6\text{Li}$
- Fast neutron detectors.
  - Bubble detectors
  - Track etch detectors
  - Thermal neutron detectors within moderators, e.g., Bonner spheres, commercial rem-meters, etc.



# 1.3 Neutron Dosimetry Challenges

- The neutrons depositing dose are not generally the neutrons generating signal
- The relationship between these is NOT constant



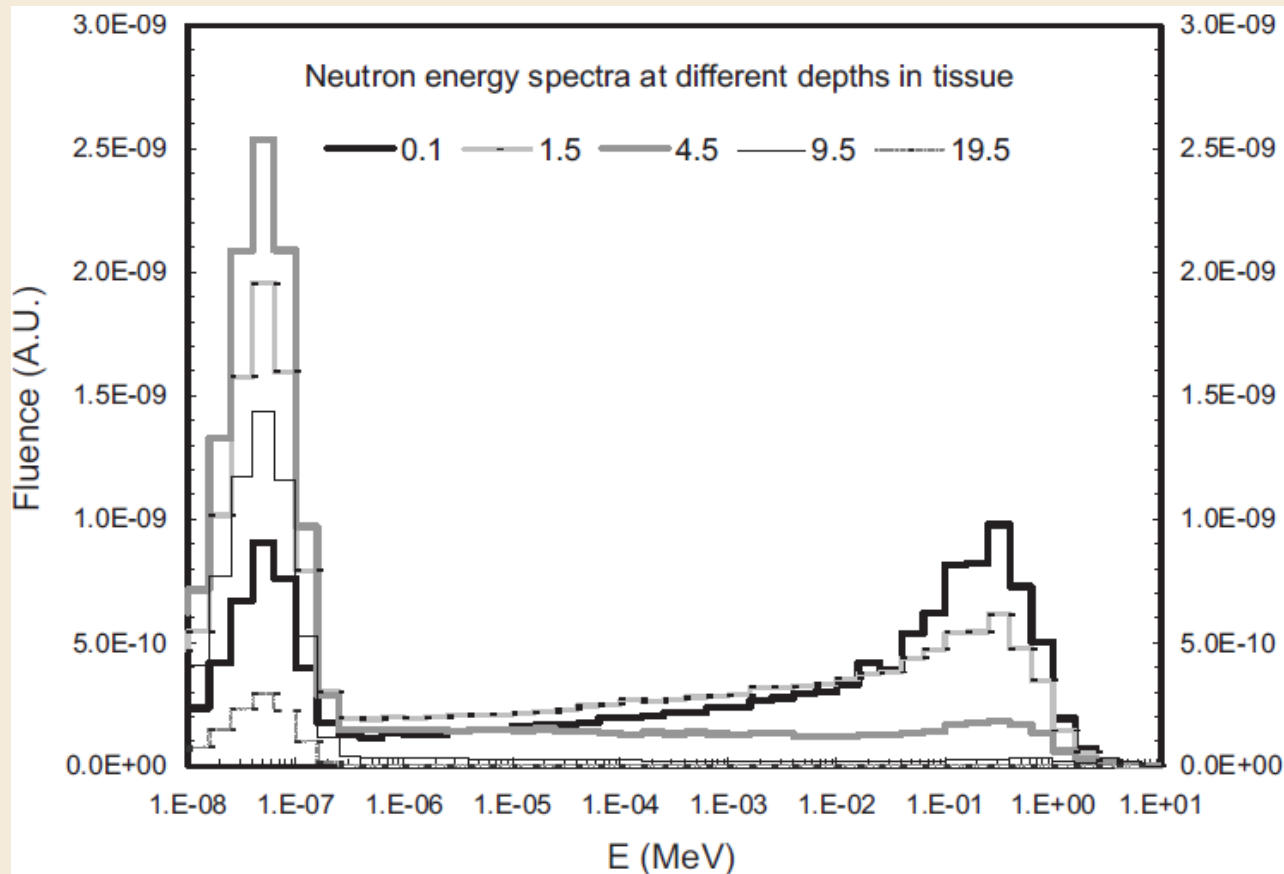
**Signal**

**Dose**

# 1.3 Neutron Dosimetry Challenges

## Phantom/Patient Measurements

- Spectrum changes dramatically and rapidly
- Can't apply a single calibration factor = **hard**



# 1.3 Neutron Dosimetry: Measurements

- Neutron dosimetry is very challenging.
- It is essential to know the spectrum you're trying to measure, and to account for any differences between this spectrum and the calibration spectrum in terms of the response of the detector.
  - Hard – requires lots of information
  - Not small errors
- In vivo/in phantom measurements are extremely challenging.
- May rely on well vetted literature.

# 1.3 Neutron Dosimetry: Measurements

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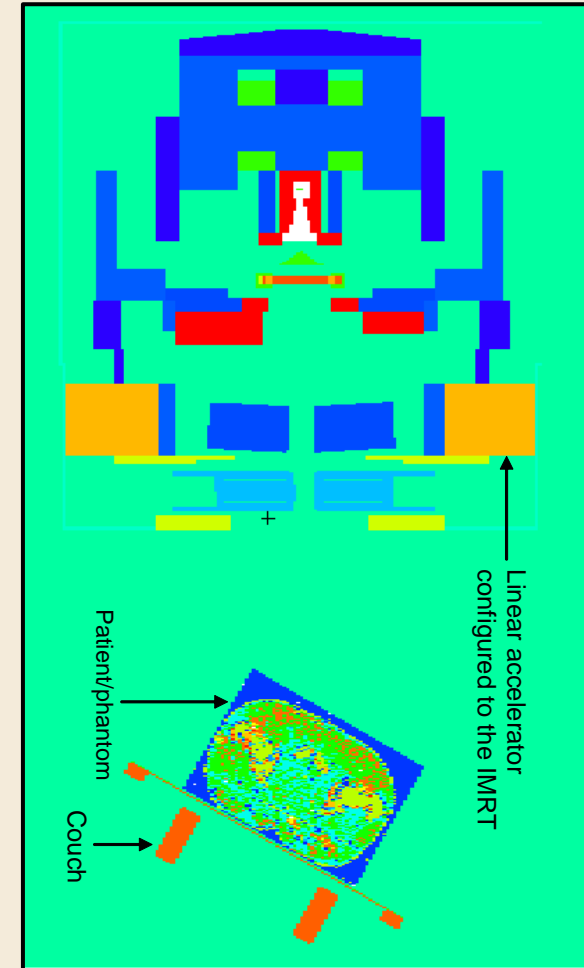


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# 1.4 Monte Carlo Photon simulations

- Can be done and provide accurate dosimetry
  - Particularly when coupled with anatomically realistic phantom
- Just a Beam-line model:
  - Accurate to ~15 cm from field edge
- Detailed head model:
  - Accurate through entire patient
- Requires detailed validation
- Not fast
- IMRT treatments may mean hundreds of individual fields to run



## 1.4 Monte Carlo

# Neutron production from x-ray therapy

- Easier simulation to calculate neutrons
  - Energy cutoff higher = faster
  - Expected precision is typically lower
- Model the entire linac head
  - Good within 10-20%
- Simple model of linac head
  - Good within ~40%
- Just beam-line components
  - Errors of 2-3 times. Don't do this.
- Validate model against good quality measurements (usually in air)



# 1. Summary

- There are several methods for assessing dose outside the treatment field
- Each one has challenges and potential pitfalls to avoid!
  
- Neutron dosimetry is most challenging
- Neutrons are typically a small component of dose equivalent (10-20%)
  - Ignored in epidemiologic studies

# TODAY'S TOPICS

## 1. Dose assessment

1. *Treatment planning system*

2. *Measurement*

3. *Neutrons*

4. *Monte Carlo*

## 2. **Dosimetric assessment for radiation epidemiology studies**

1. *Individual dosimetry*

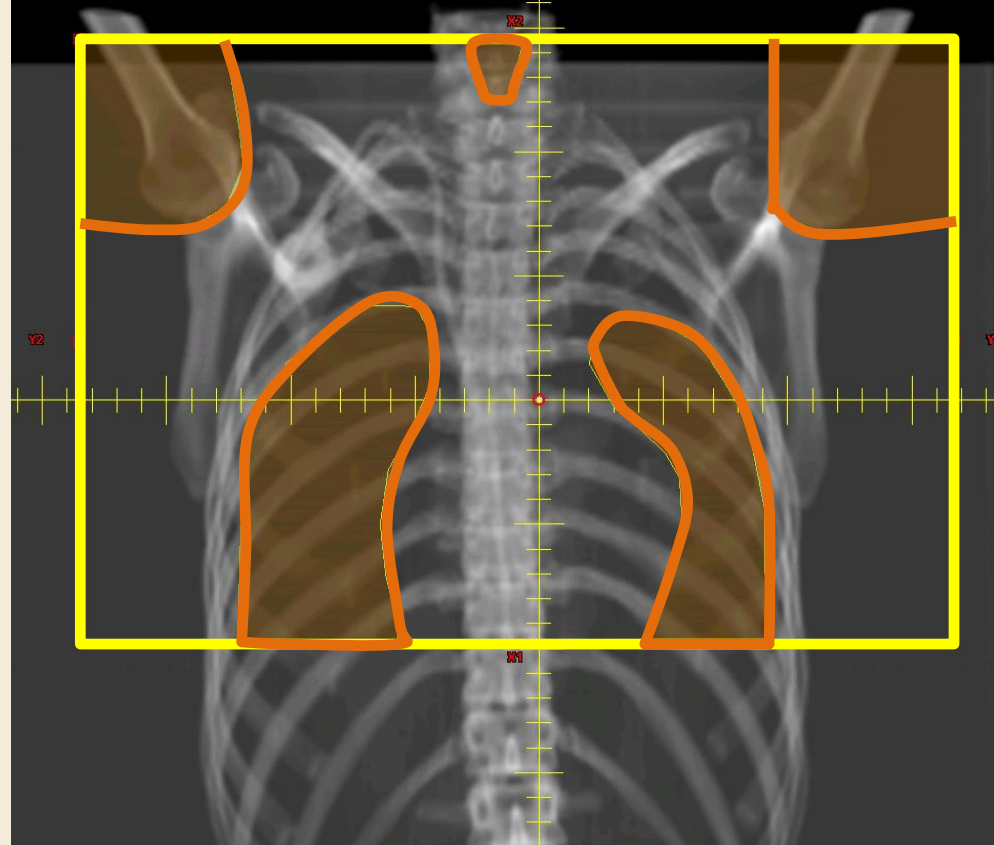
2. *Reference cases*

## 2. Dosimetric input for radiation epidemiologic studies

- This sounds very similar
  - Assess the dose to an organ of interest
  - Report it for epidemiologic consideration!
- Actually there are some very different considerations
  1. Nature of available information
  2. Quality of available information
  3. Specifics of desired information
- Must be able to implement on a large scale (1000's of patients)

## 2. Nature of Available Information

- Type of radiotherapy
- Total therapeutic dose
- Dose per fraction
- Number of beams
- Beam orientation
- Beam energy
- Radiograph with field geometry(s)



- What's not in the treatment record?

**Stray radiation dose**

**Height/weight, location of organs/second cancers....**

## 2. Nature of Available Information

- Most important detail in determining radiation dose:  
Distance from field edge
- Where does the field extend?
  - Treatment record might have DRR/port film (rarely)
  - Might have drawing. Or vague description. Or nothing.
  - Compare this with
    - Where you think the organ is
    - Separate record that has location of the tumor marked with an “X”
  - In field (100%)? On the edge (50%)? Near (10%)?
  - This transition can take only 5 cm
  - This size scale is hard to resolve if you have the patient in front of you!!

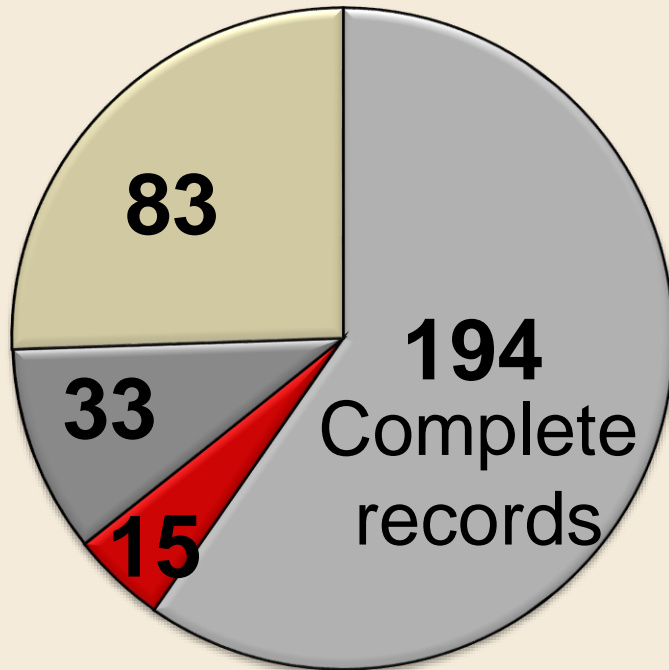
## 2. Nature of Available Information

- Might know actual size of treatment field
  - But how tall is the patient (not in patient charts, just age)?
  - What anatomy does this cover?
- Historical treatments and multi-institutional studies show a lot of variability in terms of how fields are applied – hard to make assumptions about tx.
- Messy!!!!

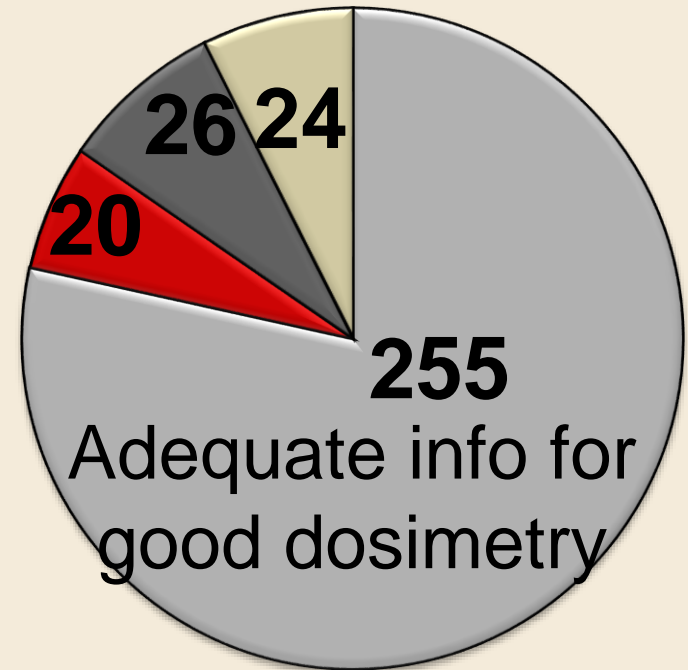
## 2. Quality of Available Information

### Is data even present?

- RT data received      RT information quality  
n=325



- Unsupported data
- Notes or summary only
- Partial Record



- Not adequate for dosimetry
- Missing information important
- Missing info not important

## 2. Nature of Desired Information

- Imagine the epidemiology study is concerned with stomach cancers after RT.
- What is the dose to the stomach?
  - If the stomach is partially inside the treatment field, the dose to different parts of the stomach will be dramatically different!
    - Mean dose? Max dose?
    - Where does the tumor originate?
- Say we generate a DVH for the stomach
  - This assumes the stomach is in the “usual” place and has the “usual” shape. This isn’t a particularly good assumption.



# TODAY'S TOPICS

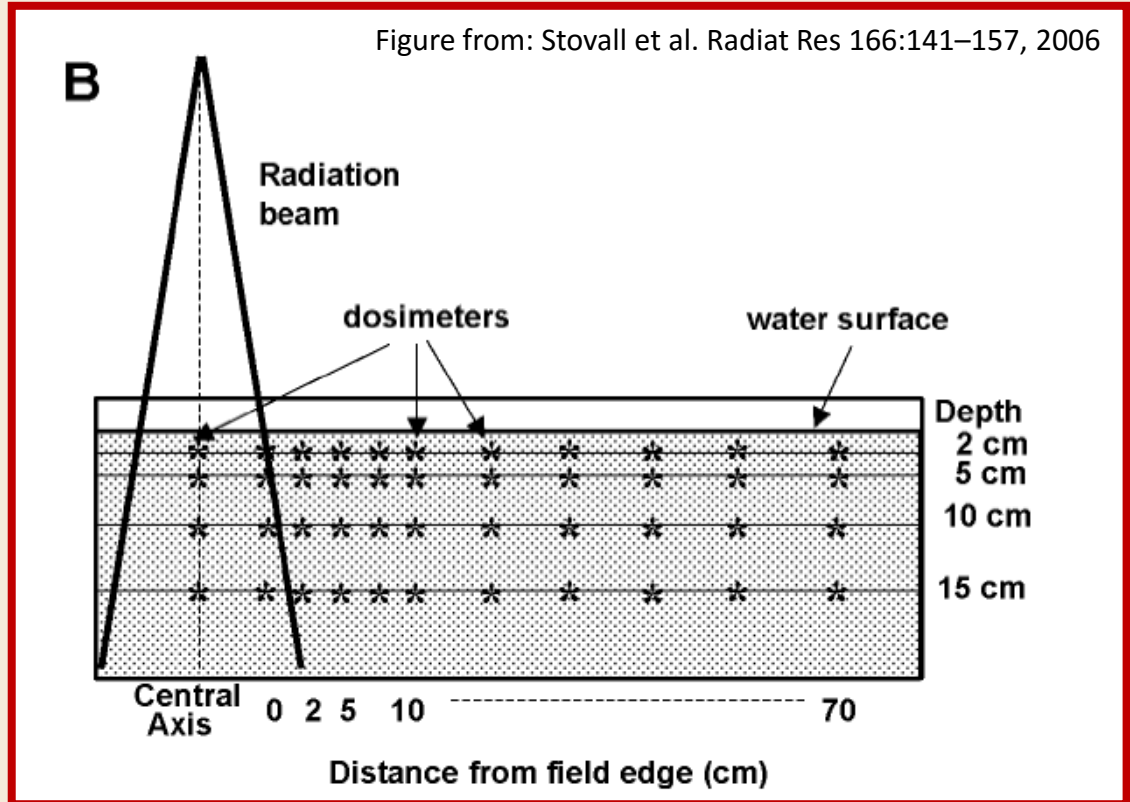
1. Dose assessment
  1. *Treatment planning system*
  2. *Measurement*
  3. *Neutrons*
  4. *Monte Carlo*
2. Dosimetric assessment for radiation epidemiology studies
  1. *Individual dosimetry*
  2. *Reference cases*

## 2.1 Individual Dosimetry

- Dosimetry for each patient case is managed and calculated individually
- Combining an analytic dosimetry model
  - Estimates dose at a given location from a given treatment field
- And a generic phantom
  - Relates geometry of tx field and location of interest
- This approach has been used for hundreds of RT-epidemiologic studies (Dr. Stovall)
  - CCSS, REB, WeCare, St. Jude life, ....

# 2.1. Analytical Model of Out-of-Field Dose

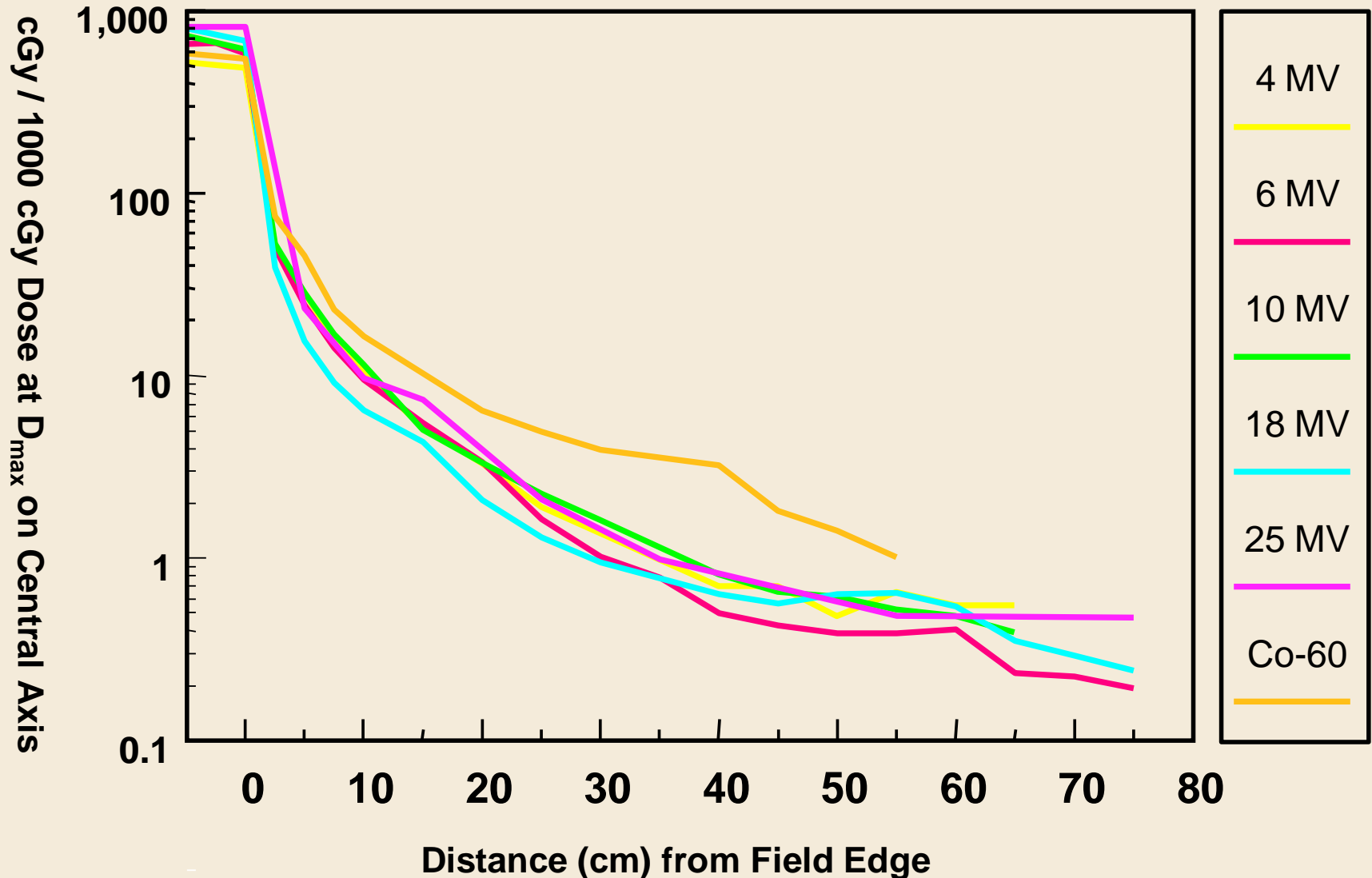
- Dose outside the treatment beam measured in large water phantom
  - Various beam energies and field sizes.



**Data fit to analytical models to derive doses at specified distances from different fields**

# 2.1 Model for total Absorbed Dose from Treatment Beams

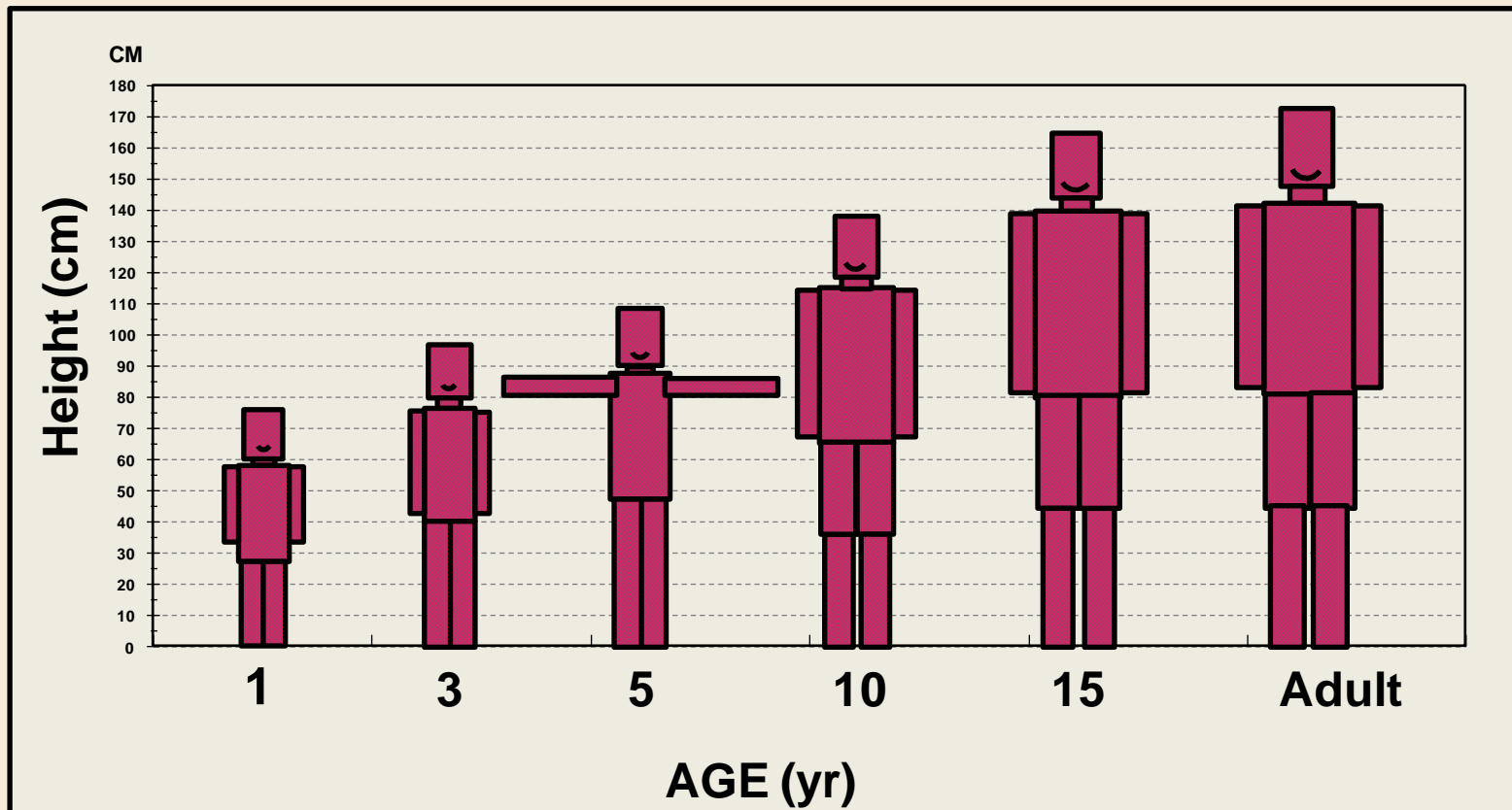
## 10x10 cm<sup>2</sup> Field Size - Various Energies



# 2.1 Mathematical Phantoms

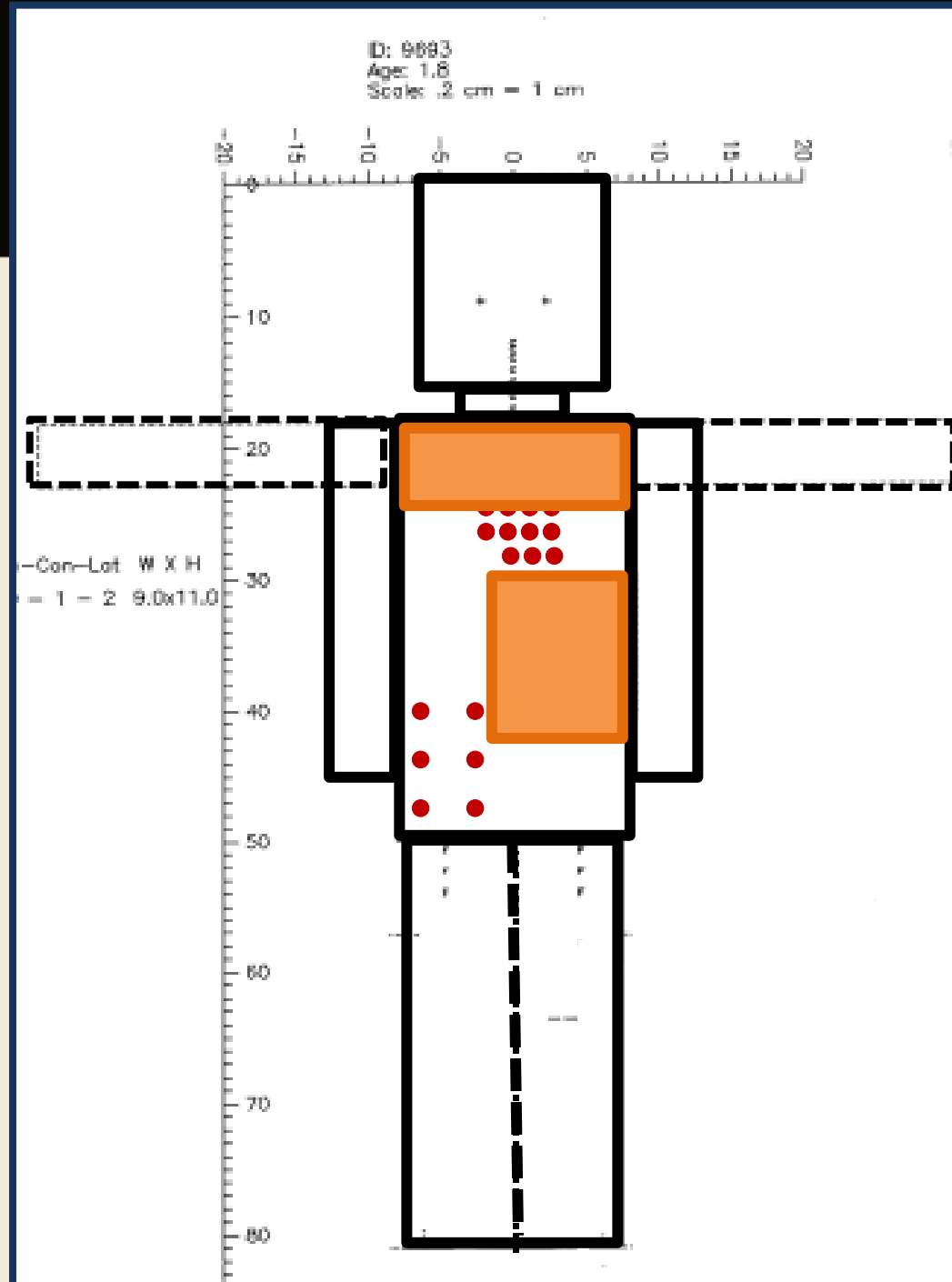
- Phantom size can be modified to represent patient of any age.

Figure from: Stovall et al. Radiat Res 166:141–157, 2006



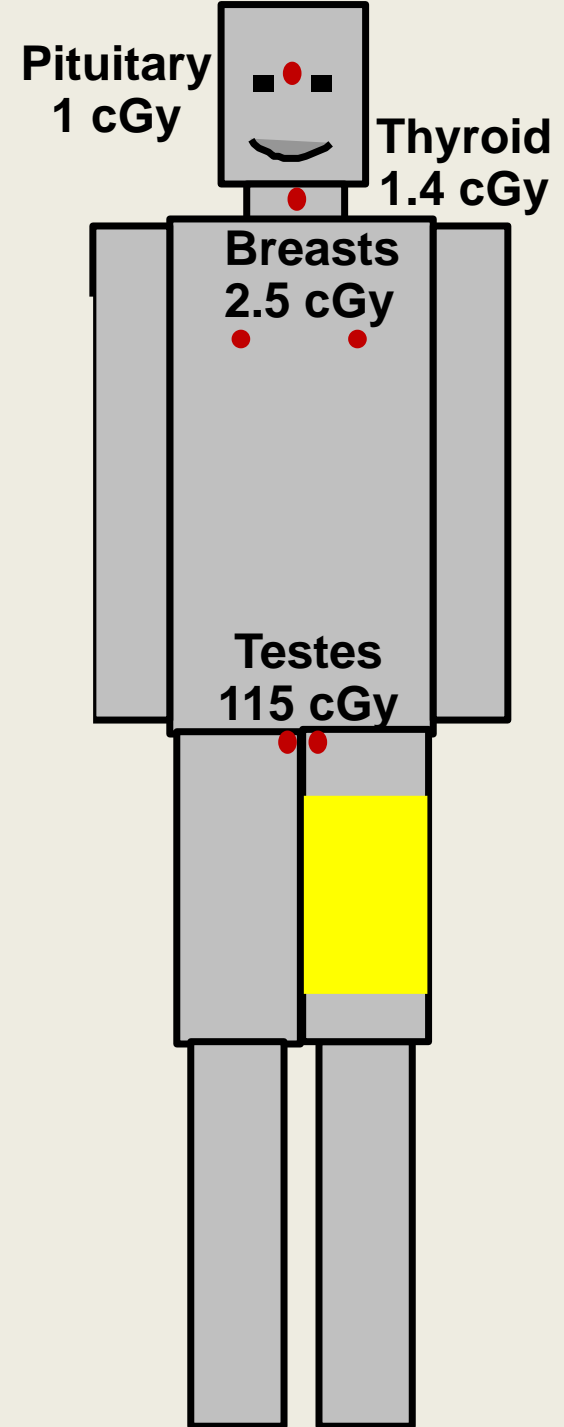
# 2.1 Mathematical Phantom

- Field can be placed in any position.
- Field geometry can be varied
- Dose calculated to point(s)
- Organs represented by a grid of points.
  - Grid can moved.
  - Grid resolution can be ↑ or ↓.



# 2.1 Mathematical Phantom Example

- **Details from RT record**
  - 16 year-old male treated for an osteosarcoma in the left thigh.
  - Field size: 12x17 cm<sup>2</sup>
  - Field orientation: AP/PA
  - Target dose: 55 Gy
  - Beam type/energy: 6 MV photons
- Mathematical phantom + analytical model used to calculate dose to out-of-field organs.
- Often must assume location of field and relative size of patient



## 2.1 Variants on this process

- Particularly variants to dose model
  - Full phantom full scatter condition.
- Analytic model for breast RT
  - tangents don't provide full scatter.
- Analytic model of skin dose from radiotherapy.
- Process is conceptually the same:
  - Abstract tx parameters of interest
  - Apply analytic model
  - Determine dose to location(s) of interest



# TODAY'S TOPICS

## 1. Dose assessment

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## 2. Dosimetric assessment for radiation epidemiology studies

1. *Individual dosimetry*

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## 2.2 Reference Case Approach

- Patients are grouped according to the nature of their treatment
  - Field orientation, modality, energy...
- Each group described by a reference treatment
- Doses are calculated for each reference treatment on a phantom (typically a single phantom).
- All patients treated according to that reference treatment are ascribed that dose.
- This approach has been used in many studies

## 2.2 Reference Case Dosimetry

- Example study: cardiac toxicity following breast RT
- Radiotherapy treatments categorized according to regimen:
  - laterality, field arrangement, prescription dose(s), dose/fx.
- 22 standard treatment regimens.
  - Each patient was classified to a particular regimen based on data in treatment chart.

## 2.2 Reference treatments

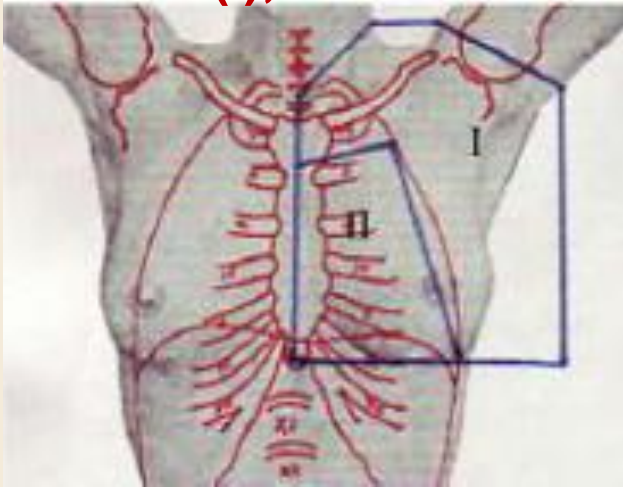
**Wide Tangential Pair**



**Tangential Pair to Midline**



**Lat thorax (I), e-IMC and e-CW (II)**

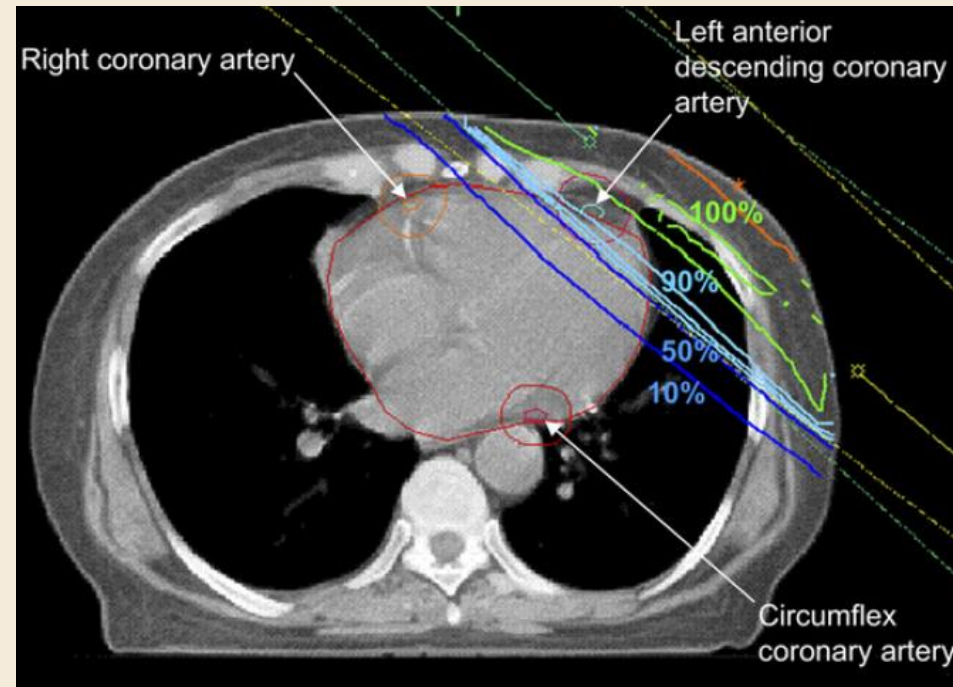


**Lat thorax (I), e-IMC (II) and e-CW (III)**



## 2.2 Reference dose recalculation

- The different RT regimes were reconstructed on a CT scan of typical patient of average build.
  - Heart and Coronary arteries were contoured
  - DVH were used to determine mean heart dose for each regime.
  - Heart doses were “assigned” to all patients with that regimen classification



Taylor *et al.* IJORBP 2007

**TPS doesn't work for stray radiation doses!**

**Could apply an analytic model to determine these doses**

## 2. Dosimetry for epidemiology summary

- Both systems struggle to define field edge
  - Charts typically don't define it well
- Both systems rely on “average” patient size and typical patient anatomy
- Both systems suffer from incomplete patient records
- Individual dosimetry better captures differences between patients
- Reference case approach better manages dosimetry within the reference case (and may be the only option if limited chart information is available)
- These differences are likely small compared to the larger uncertainty items above

# Final thoughts

- Assessing the dose outside the treatment field has challenges at the best of times
- Retrospective radio-epi studies are NOT the best of times
  - Incomplete information
- The better prospective planning we can do, the better the dosimetric data we will generate.
  - Invest in the future to ensure quality data
  - Particularly as treatments become more complex



**End**

## Thanks

- Marilyn Stovall PhD
- Rebecca Howell PhD
- Jessie Huang PhD
- Sarah Scarborough PhD
- Kiley Pulliam
- Susan Smith
- Rita Weathers





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- Taylor CW, Nisbet A, McGale P, et al. Cardiac doses from Swedish breast cancer radiotherapy since the 1950s. *Radiother Oncol* 2009;90:127-35.